

The comparison of torque values in two types of miniscrews placed in rabbits: tapered and cylindrical shapes

- Preliminary study

Kyung-Ho Kim, DDS, MS, PhD,^a Choorjung Chung, DDS, PhD,^b Hyun-Mi Yoo, DDS, MS, PhD,^c
Dong-Sung Park, DDS, MS, PhD,^d In-Sung Jang, BA,^e Seung-Hyun Kyung, DDS, MS, PhD^f

Objective: This study compared the stability of cylindrical miniscrews (Cy, 7 mm in length) with that of tapered miniscrews (Ta, 5 mm in length), using torque values to determine if the healing time before loading affects the stability of the miniscrew and if the insertion torque is associated with the removal torque measured after a few weeks of healing. **Methods:** Ta and Cy with different thread lengths were placed in the tibiae of 12 female New Zealand white rabbits (body weight: 3.0 - 3.5 kg), and the maximum insertion torque values (ITV) were measured. No orthodontic forces were applied so as to allow us to determine the pure effects of the different shapes. After 3 different healing periods (2, 4, and 6 weeks), maximum removal torque values (RTV) were measured immediately before the rabbits were sacrificed. **Results:** No miniscrews were loosened. There were no significant differences in ITV or RTV between the Ta and Cy nor were there any significant differences in the ITV and RTV between the 3 groups, which had different healing periods. There was a correlation between the ITV and RTV. **Conclusions:** Shorter Ta showed similar stability as Cy, as determined by torque values. This result strongly suggests that the tapered shape is more advantageous than the cylindrical shape. The RTV did not increase significantly over time. It is recommended that a miniscrew be loaded immediately; waiting a few weeks before loading should be avoided. The correlation between the ITV and RTV suggests that the ITV can be used to estimate a screw's future stability. (*Korean J Orthod* 2011;41(4):280-287)

Key words: Tapered shape, Torque, Miniscrew, Stability

^aProfessor, ^bAssistant Professor, Department of Orthodontics, Gangnam Severance Dental Hospital.

^cProfessor, ^dProfessor, Department of Conservative Dentistry, The Institute of Oral Health & Science, Samsung Medical Center, Sungkyunkwan University School of Medicine.

^eVeterinarian, Samsung Biomedical Research Institute, Laboratory Animal Research Center.

^fAssociate Professor, Department of Orthodontics, The Institute of Oral Health & Science, Samsung Medical Center, Sungkyunkwan University School of Medicine.

Corresponding author: **Seung-Hyun Kyung.**

Department of Orthodontics, The Institute of Oral Health & Science, Samsung Medical Center, Sungkyunkwan University School of Medicine, 50 Irwon-dong, Gangnam-gu, Seoul 135-710, Korea.

+82 2 569 3328; e-mail, shkyung@gmail.com.

Received April 5, 2010; Last Revision December 3, 2010;

Accepted December 6, 2010.

<http://dx.doi.org/10.4041/kjod.2011.41.4.280>

INTRODUCTION

Since the introduction of miniscrews for orthodontic anchorage, various tooth movements that had been previously thought impracticable are now considered possible. For example, the skeletal open bite, which has been corrected with combined surgery of the maxilla and mandible, can be treated with miniscrews without orthognathic surgery.¹⁻³ Recently, it was reported that space can be gained by molar distalization with miniscrews a non-extraction treatment.⁴⁻⁶ Although the treatment results with miniscrews are remarkable, this treatment raises challenges not encountered before.

Among these, frequent loosening is one of the main challenges that needs to be overcome. The osseointegrated dental implant used to restore missing teeth has undergone various modifications to increase the success rate, such as changes in diameter, length, pitch, and thread shape.^{7,8} However, efforts to enhance the stability of orthodontic miniscrews with design modifications have just begun. One approach is to place a tapered miniscrew based on the assumption that the tapered shape might affect initial stability.^{9,10} The tapered shape pushes out the bone around it as it is inserted, inducing compressive pressure on the cortical bone around the neck where the stress is mainly concentrated when elastics are applied.¹¹ The effect of a tapered shape can be considered an advantage or disadvantage in terms of stability. It is an advantage if it increases the bone density around the neck, enhancing stability.^{10,12-14} However, it is a disadvantage if it causes excessive pressure, sufficient to inhibit blood flow to the osteocytes within the bone, leading to cell death and bone necrosis.¹⁵

Another way of increasing miniscrew stability is to wait 2 - 4 weeks for osseointegration. Animal studies^{16,17} suggested that miniscrews might undergo osseointegration. However, some studies recommend placing a load immediately without waiting for healing.^{10,18-20} Moreover, studies revealed no significant differences between the groups of delayed loading and immediate loading.²¹⁻²⁴

This study compared the stability, as determined by torque values, of a cylindrical miniscrew with that of a tapered one in order to determine if the tapered shape enhances miniscrew stability and to determine if the healing time before loading affects the stability of the miniscrew. We also aimed to determine if the insertion torque is associated with the removal torque, which is measured after a few weeks of healing.

MATERIAL AND METHODS

This study was reviewed and approved by the Institutional Animal Care and Use Committee (IACUC) of Samsung Biomedical Research Institute (SBRI). The SBRI is an Association for the Assessment and Accreditation of Laboratory Animal Care International

(AAALAC International) accredited facility and abides by the rules of the Institute of Laboratory Animal Resources (ILAR) guide.

Miniscrews

Two types of miniscrews, tapered and cylindrical, were made from BMK (Orthoplast, Biomaterials Korea Inc., Seoul, Korea) so that they generated similar maximum insertion torque values (ITVs), as determined by preliminary studies performed on artificial bone blocks. This was possible because the tapered design had a higher torque value than the cylindrical design,²⁵ even if the thread lengths differed. The thread length of the cylindrical miniscrews (Cy) was 7 mm. Cy are the most popular orthodontic miniscrews on the market. The tapered miniscrews (Ta) had a thread length of 5 mm; tapering was more than usual in order to amplify the effect of this shape (Fig 1).

Animals and anesthesia

Twelve female New Zealand white rabbits (body weight: 3.0 - 3.5 kg) were used in this study. The rabbits were anesthetized with xylazine (5 mg/kg ad-

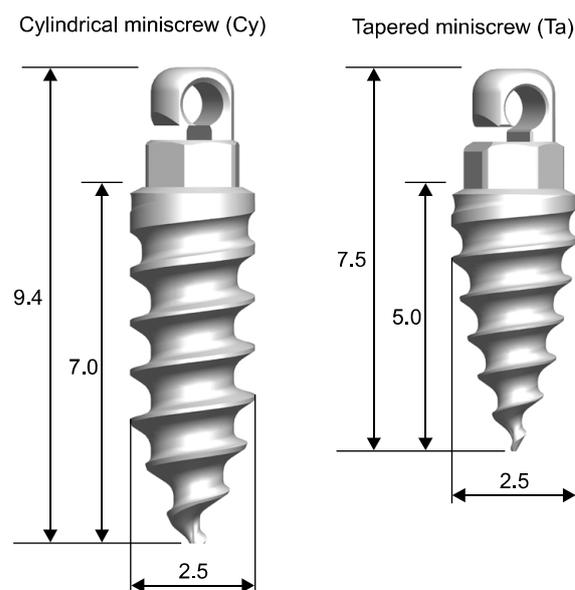


Fig 1. Diameters and thread lengths of 2 types of miniscrews.

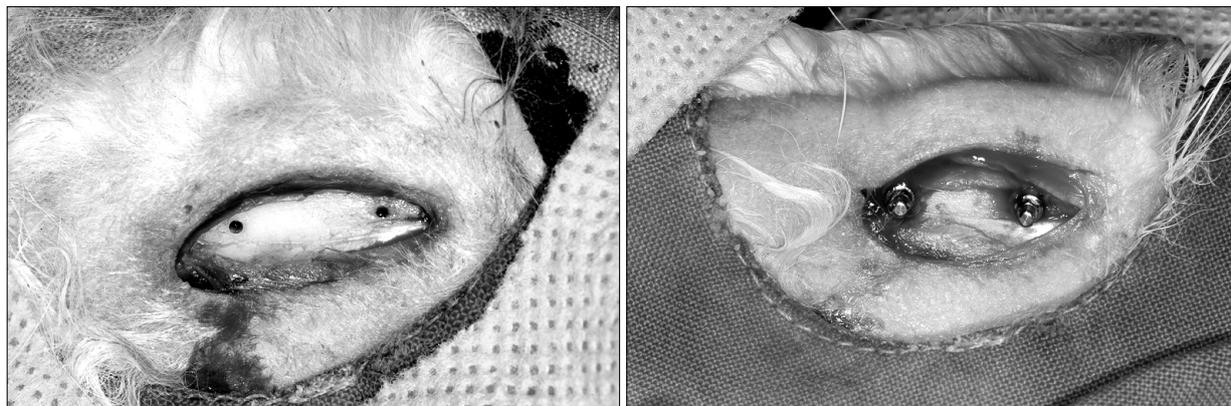


Fig 2. Two miniscrews were placed into each tibia after making 1 mm (diameter) pilot holes with a distance of 15 mm between them.

ministered intramuscularly) and ketamine (35 mg/kg administered intramuscularly). Next, 1 ml of 2% lidocaine was injected into the surgical regions of the tibia for additional local anesthesia.

Measurement of maximum insertion torque value (ITV)

Prior to surgery, the regions to be operated upon were shaved and decontaminated with iodine and 70% ethanol. The tibia was exposed by incising through the skin, fascia, and periosteum. Although the miniscrews were drill-free types, a preliminary study found that tibia fractures occasionally occurred without pilot holes when the miniscrews were inserted; the fractures were attributed to the cortical bone of the rabbit tibia being too hard. Pilot holes with a 1 mm diameter were drilled at 30 rpm, using a bone drill on the body of the tibia under saline irrigation to minimize the amount of heat. The distance between the 2 holes was approximately 15 mm. Two types of miniscrews, Cy and Ta, were placed only until the upper ends of the thread were flush with the external surfaces of the tibia bone (Fig 2). In other words, 5 mm and 7 mm of thread in the Ta and Cy, respectively, was inserted into the bone. Two Cy were placed on one side of the 2 legs, and 2 Ta were placed on the other side. ITV was measured using a digital torque driver (DI-5-RL2; Sugisaki Meter Co., LTD 5085-23, Ibaraki, Japan) in Ncm units (Fig 3). No orthodontic forces were applied

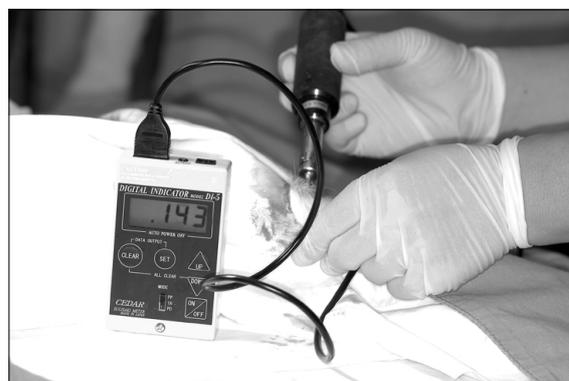


Fig 3. The digital torque gauge used in this study.

in order to observe the pure effects of the different designs. Surgical sites were closed in layers. The muscle, fascia, and internal dermal layers were sutured, while the outer dermis was sutured for primary closure. After surgery, all rabbits were administered the antibiotic, Baytril, at a dose of 10 mg/kg and ketoprofen at a dose of 1 mg/kg.

Measurements of maximum removal torque value (RTV)

There were 3 groups of 4 rabbits each. Rabbits were grouped according to the healing period (2, 4, and 6 weeks). Four rabbits were sacrificed at the end of each healing period. The maximum RTVs were obtained while the rabbits were still alive in order to reproduce the clinical situation. The rabbits were anesthetized

with an intramuscular injection of ketamine (35 mg/kg) and xylazine (5 mg/kg). The maximum RTV was measured using a digital torque gauge (Fig 3) and recorded. After confirming the RTV, the anesthetized rabbits were euthanized using KCl.

Statistical analysis

For comparisons between the 2 types of miniscrews and between groups, due to small sample size, median regression adjusting for location, type of miniscrew, healing period, and subject was used. *p*-values were corrected using Bonferroni's method, adjusting for inflated type I error. The correlation between ITV and RTV was also tested using median regression, adjusting for type, location, and healing periods. A *p*-value of <0.05 was considered significant.

RESULTS

All rabbits recovered from the anesthesia without complications, and all miniscrews were found to be stable at the end of the 3 experimental periods. Upon re-exposure, some of the miniscrews were partially covered with bone. The bone over the head of the miniscrews was removed with a scalpel before measuring the RTV with a torque gauge in order to avoid biased values.

There was no significant difference between Ta and Cy in terms of the median ITVs or RTVs within each group. The median (Q1-Q3) total ITV in Ta and in Cy were 15.8 (10.7 - 23.5) Ncm and 15.6 (10.4 - 24.0) Ncm, respectively, and the median (Q1-Q3) total RTV in Ta and in Cy were 5.3 (4.3 - 7.6) Ncm and 5 (3.9 - 7.9) Ncm, respectively. Analysis using median regression adjusting for location and healing time effects

Table 1. Difference in torque values between the 2 types of miniscrews

| | Time | Location | N | Ta median (Q1-Q3) | Cy median (Q1-Q3) | <i>p</i> -value | | | |
|-----|------|----------|---|--------------------|--------------------|-----------------|------|-----|-------|
| | | | | | | Ta/Cy* | Ta† | Cy§ | Total |
| ITV | 2 w | P | 4 | 13.6 (10.8 - 16.0) | 11.9 (9.9 - 12.9) | 1.0 | - | - | - |
| | | D | 4 | 22.3 (18.8 - 26.7) | 23.2 (22.6 - 26.1) | | | | |
| | 4 w | P | 4 | 12.6 (10.7 - 12.7) | 12.0 (10.4 - 13.0) | 1.0 | 1.0 | 1.0 | 1.0 |
| | | D | 4 | 29.7 (25.6 - 33.7) | 29.0 (27.5 - 30.0) | | | | |
| | 6 w | P | 4 | 8.7 (7.8 - 10.8) | 9.0 (7.3 - 11.9) | 1.0 | 1.0 | 1.0 | 0.87 |
| | | D | 4 | 23.5 (20.3 - 24.4) | 21.7 (18.0 - 25.4) | | | | |
| | | | | 0.68† | | | | | |
| RTV | 2 w | P | 4 | 5.2 (4.6 - 5.3) | 3.9 (2.2 - 5.9) | 1.0 | - | - | - |
| | | D | 4 | 7.8 (7.0 - 10.9) | 8.8 (6.2 - 9.7) | | | | |
| | 4 w | P | 4 | 4.7 (3.4 - 5.5) | 4.0 (3.6 - 4.2) | 1.0 | 0.89 | 1.0 | 1.0 |
| | | D | 4 | 6.8 (4.1 - 8.1) | 7.8 (6.2 - 8.5) | | | | |
| | 6 w | P | 4 | 4.2 (3.8 - 4.8) | 3.7 (2.4 - 6.7) | 0.23 | 1.0 | 1.0 | 1.0 |
| | | D | 4 | 6.9 (4.6 - 11.5) | 5.3 (4.4 - 6.7) | | | | |
| | | | | 0.41† | | | | | |

ITV, Insertion torque value; RTV, removal torque value; Ta, tapered miniscrew; Cy, cylindrical miniscrew. Location P: Proximal area of the tibia, D: distal area of the tibia. N: numbers of miniscrews. Note-Data are presented as the median (interquartile range). Median regression was used. *Comparison between Ta and Cy, adjusting for location effect each time; †Comparison between Ta and Cy, adjusting for location and time effects in total; ‡Comparison between times (2 w vs. 4 w, 2 w vs. 6 w), adjusting for location effect in Ta; §Comparison between times (2 w vs. 4 w, 2 w vs. 6 w), adjusting for location effect in Cy; ||Comparison among times (2 w vs. 4 w, 2 w vs. 6 w), adjusting for location and type effects in total.

Table 2. Association of RTV

| | Estimate | Standard error | t value | p-value |
|-------------|----------|----------------|---------|--------------------|
| ITV (Ta) | 0.05 | 0.19 | 0.25 | 1.0* |
| ITV (Cy) | 0.16 | 0.17 | 0.95 | 0.704* |
| ITV (Total) | 0.17 | 0.07 | 2.38 | 0.022 [†] |

RTV, Removal torque value; ITV, insertion torque value; Ta, tapered miniscrew; Cy, cylindrical miniscrew. Note-Median regression was used. *Adjusting for time and location effects; [†]Adjusting for time, type, and location effects.

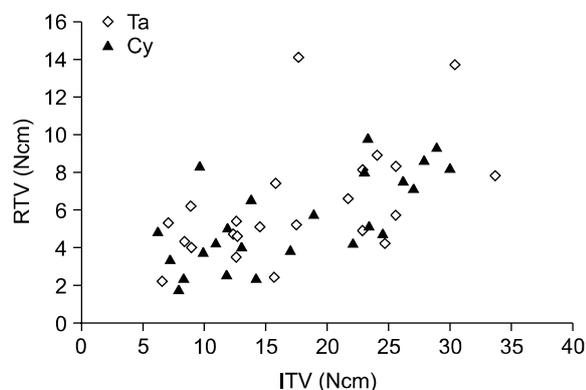


Fig 4. Scatter plot of the RTV and ITV of 48 miniscrews. Ta, Tapered miniscrew; Cy, cylindrical miniscrew; RTV, removal torque value; ITV, insertion torque value.

showed that the difference between Ta and Cy was not significant in terms of total ITV ($p = 0.68$) and total RTV ($p = 0.41$) (Table 1).

There was no significant difference between healing periods (2 weeks vs. 4 weeks, 2 weeks vs. 6 weeks) within Ta or Cy groups (Table 1). Further, the correlation between the ITVs and RTVs was significant ($p = 0.022$) (Table 2, Fig 4).

DISCUSSION

Torque is closely related to the factors that determine the stability of miniscrews, such as bone density^{26,27} and cortical bone thickness.²⁸ In addition, the torque value is frequently used as an indirect method to assess the stability of an implant or miniscrew.^{9,29-32}

There are 2 types of miniscrews available: tapered and cylindrical. However, there is limited information about their differences.

Lim et al.³³ reported that there was a significant increase in insertion torque with increasing screw diameter. There were no significant differences in the total ITV and RTV between Ta and Cy as well as in the ITV and RTV within each group (Table 1). The similar ITV was intended from the study design and meant that the experimental procedures had been carried out appropriately.

The length and diameter are 2 major factors that determine the stability of a miniscrew.^{34,35} The median (Q1-Q3) RTV of Ta [5.3 (4.3 - 7.6) Ncm] was comparable to that of Cy [5 (3.9 - 7.9) Ncm]. The RTV of Ta should be lower than that of Cy if bone cells are injured as a result of too much pressure originating from the tapered shape. However, Ta and Cy showed similar stability, even though Ta were 2 mm shorter than Cy. This stability was attributed to the similar diameter of the two types at the level of the cortical bone, which is believed to provide the miniscrews with the main mechanical retention. Ta might not cause excessive pressure to the bone tissue, and they induce a similar bone reaction to Cy. The shorter shank of Ta could be advantageous over Cy because the proximity of a miniscrew to the root is a major risk factor for the failure of screw anchorage.²¹ The longer thread of Cy increases the likelihood of root contact. Therefore, Ta could be more advantageous in terms of less root damage and better stability. Although the tapered shape increased the crestal strain,⁷ some in vitro^{13,25} and animal studies^{9,10} have reported that the tapered design is more advantageous than the cylindrical design in terms of mechanical and biological stability.

Some orthodontists load the miniscrew immediately, whereas others do not. The waiting period before loading varies according to the clinician. Therefore, it is necessary to determine which of the 2 loading protocols is more beneficial for miniscrew stability, and how long a waiting period is appropriate if delayed loading is better. Early loading might decrease the level of osseointegration of orthodontic mini-implants.¹⁷ Some studies suggest that the machined surface of pure titanium or titanium alloy could be integrated with

bone.^{30,36} However, other researchers²⁰⁻²⁴ could not find any influence of a waiting period before loading on the stability of orthodontic miniscrews. These results are in accordance with those of the present study, which found no differences between the mean RTV of the 3 groups, suggesting that no osseointegration occurred with time. Roberts reported 6 weeks to be an adequate healing period in rabbits prior to loading in order to attain rigid stability.³⁷ If osseointegration progresses with healing time, the RTV in this study would increase with time, as reported by Klokkevold et al.³⁰ However, the RTV in this study was similar in all the 3 groups (Table 1), which is consistent with some studies.^{18,24} According to Morais et al.,¹⁶ who examined rabbits, there was no increase in the RTV when the healing period was between 1 and 4 weeks. However, the RTV increased significantly after 12 weeks. In the present study, the 5 miniscrews circled with a red line in Fig 4, showed relatively higher RTVs than ITVs as compared with the other miniscrews. Four out of the 5 miniscrews were included in the group that was allowed a healing period of 6 weeks, and the remaining one was from the 4-week group, which strongly suggests integration between the bone and miniscrews. Therefore, orthodontic miniscrews with a machined surface of Ti-6Al-4V titanium alloy could be integrated with bone experimentally, as reported in Morais' study.¹⁶ On the other hand, a healing period of more than 6 weeks to improve the stability of miniscrews is unsuitable for orthodontic patients. The results of other studies and the present study suggest that it would be difficult to obtain osseointegration in humans within a few weeks. Therefore, it is not recommended to wait for a few weeks before applying a force, expecting better fixation of the miniscrew. The orthodontic miniscrew is not made primarily of pure titanium. Moreover, it is not surface-treated or packed as a prosthetic dental implant, and the entire placement procedure differs from that of a prosthetic dental implant. Placing a low-intensity load immediately after placing early orthodontic static loads did not affect the mini-implant's performance.³⁸

There have been no objective references to determine the future stability of a miniscrew. Clinicians are only able to presume its stability on the basis of

the resistance carried to their hands through the driver handle. Although Resonance Frequency Analysis (RFA),³⁹⁻⁴¹ periotest,⁴² and insertion torque^{26,40} measurements are used to assess the stability of an osseointegrated prosthetic implantor miniscrew, none of these are the gold standard. The RTV is closely related to the stability of miniscrews rather than to the ITV because it reveals the degree of fixation that has occurred after the bone reactions that occurred during healing. Median regression adjusting for time, type, and location effects revealed a correlation between the ITV and RTV ($p = 0.022$), which means the RTV increased with the ITV. There was, however, no significant correlation between each tapered and cylindrical miniscrew. Scatter plots for Ta and Cy demonstrated similar patterns (Fig 4). The reason, therefore, for significant correlation between the ITV and RTV in 48 miniscrews seemed to be the large sample size. It was presumed that ITV might be an indicator of the future stability of a miniscrew. This is not consistent with the results obtained by Motoyoshi,¹¹ who reported that the optimal placement torque to raise the success rate of a mini-implant ranges from 5 to 10 Ncm. and Okuyama⁴³ in accordance with Ottoni et al.⁴⁴ reported that the potential risk decreased with increasing ITV, and Song et al.²⁵ who stated that the RTV increases as the ITV increases.

This study had some limitations. The first was that the healing time appeared to be too short to observe all the changes occurring at the interface between the miniscrew and bone, even though a 6-week healing period in rabbits is equivalent to approximately 18 weeks in humans.³⁷ The second was that this study did not determine if the stability of miniscrews varied with design in the case of force application. Third, a histomorphologic analysis should have been performed to compare the precise differences in bone reactions to Ta and Cy.

CONCLUSION

1. The shorter Ta showed similar stability to the Cy, which strongly suggests that the tapered shape is more advantageous than the cylindrical shape.
2. RTV did not increase significantly over time. It is

recommended that a miniscrew be loaded immediately; waiting a few weeks before loading should be avoided.

3. There was a correlation between the ITV and RTV, indicating that the ITV can be used as an indicator of the future stability of a miniscrew.

REFERENCES

1. Umemori M, Sugawara J, Mitani H, Nagasaka H, Kawamura H. Skeletal anchorage system for open-bite correction. *Am J Orthod Dentofacial Orthop* 1999;115:166-74.
2. Park HS, Kwon OW, Sung JH. Nonextraction treatment of an open bite with microscrew implant anchorage. *Am J Orthod Dentofacial Orthop* 2006;130:391-402.
3. Choi KJ, Choi JH, Lee SY, Ferguson DJ, Kyung SH. Facial improvements after molar intrusion with miniscrew anchorage. *J Clin Orthod* 2007;41:273-80.
4. Sugawara J, Kanzaki R, Takahashi I, Nagasaka H, Nanda R. Distal movement of maxillary molars in nongrowing patients with the skeletal anchorage system. *Am J Orthod Dentofacial Orthop* 2006;129:723-33.
5. Kyung SH, Hong SG, Park YC. Distalization of maxillary molars with a midpalatal miniscrew. *J Clin Orthod* 2003;37:22-6.
6. Kyung SH, Lee JY, Shin JW, Hong C, Dietz V, Gianelly AA. Distalization of the entire maxillary arch in an adult. *Am J Orthod Dentofacial Orthop* 2009;135(4 Suppl):S123-32.
7. Petrie CS, Williams JL. Comparative evaluation of implant designs: influence of diameter, length, and taper on strains in the alveolar crest. A three-dimensional finite-element analysis. *Clin Oral Implants Res* 2005;16:486-94.
8. Renouard F, Nisand D. Impact of implant length and diameter on survival rates. *Clin Oral Implants Res* 2006;17 Suppl 2:35-51.
9. O'Sullivan D, Sennerby L, Meredith N. Influence of implant taper on the primary and secondary stability of osseointegrated titanium implants. *Clin Oral Implants Res* 2004;15:474-80.
10. Yano S, Motoyoshi M, Uemura M, Ono A, Shimizu N. Tapered orthodontic miniscrews induce bone-screw cohesion following immediate loading. *Eur J Orthod* 2006;28:541-6.
11. Motoyoshi M, Hirabayashi M, Uemura M, Shimizu N. Recommended placement torque when tightening an orthodontic mini-implant. *Clin Oral Implants Res* 2006;17:109-14.
12. Akkocaoglu M, Uysal S, Tekdemir I, Akca K, Cehreli MC. Implant design and intraosseous stability of immediately placed implants: a human cadaver study. *Clin Oral Implants Res* 2005;16:202-9.
13. Sakoh J, Wahlmann U, Stender E, Nat R, Al-Nawas B, Wagner W. Primary stability of a conical implant and a hybrid, cylindrical screw-type implant in vitro. *Int J Oral Maxillofac Implants* 2006;21:560-6.
14. Wilmes B, Rademacher C, Olthoff G, Drescher D. Parameters affecting primary stability of orthodontic mini-implants. *J Orofac Orthop* 2006;67:162-74.
15. Ueda M, Matsuki M, Jacobsson M, Tjellström A. Relationship between insertion torque and removal torque analyzed in fresh temporal bone. *Int J Oral Maxillofac Implants* 1991;6:442-7.
16. Morais LS, Serra GG, Muller CA, Andrade LR, Palermo EF, Elias CN, et al. Titanium alloy mini-implants for orthodontic anchorage: immediate loading and metal ion release. *Acta Biomater* 2007;3:331-9.
17. Zhao L, Xu Z, Yang Z, Wei X, Tang T, Zhao Z. Orthodontic mini-implant stability in different healing times before loading: a microscopic computerized tomographic and biomechanical analysis. *Oral Surg Oral Med Oral Pathol Oral Radiol Endod* 2009;108:196-202.
18. Deguchi T, Takano-Yamamoto T, Kanomi R, Hartsfield JK Jr, Roberts WE, Garetto LP. The use of small titanium screws for orthodontic anchorage. *J Dent Res* 2003;82:377-81.
19. Luzzi C, Verna C, Melsen B. A prospective clinical investigation of the failure rate of immediately loaded mini-implants used for orthodontic anchorage. *Prog Orthod* 2007;8:192-201.
20. Woods PW, Buschang PH, Owens SE, Rossouw PE, Opperman LA. The effect of force, timing, and location on bone-to-implant contact of miniscrew implants. *Eur J Orthod* 2009;31:232-40.
21. Kuroda S, Sugawara Y, Deguchi T, Kyung HM, Takano-Yamamoto T. Clinical use of miniscrew implants as orthodontic anchorage: success rates and postoperative discomfort. *Am J Orthod Dentofacial Orthop* 2007;131:9-15.
22. Miyawaki S, Koyama I, Inoue M, Mishima K, Sugahara T, Takano-Yamamoto T. Factors associated with the stability of titanium screws placed in the posterior region for orthodontic anchorage. *Am J Orthod Dentofacial Orthop* 2003;124:373-8.
23. Park HS, Jeong SH, Kwon OW. Factors affecting the clinical success of screw implants used as orthodontic anchorage. *Am J Orthod Dentofacial Orthop* 2006;130:18-25.
24. Chen YJ, Chen YH, Lin LD, Yao CC. Removal torque of miniscrews used for orthodontic anchorage--a preliminary report. *Int J Oral Maxillofac Implants* 2006;21:283-9.
25. Song YY, Cha JY, Hwang CJ. Mechanical characteristics of various orthodontic mini-screws in relation to artificial cortical bone thickness. *Angle Orthod* 2007;77:979-85.
26. Friberg B, Sennerby L, Roos J, Johansson P, Strid CG, Lekholm U. Evaluation of bone density using cutting resistance measurements and microradiography: an in vitro study in pig ribs. *Clin Oral Implants Res* 1995;6:164-71.
27. Ikumi N, Tsutsumi S. Assessment of correlation between computerized tomography values of the bone and cutting torque values at implant placement: a clinical study. *Int J Oral Maxillofac Implants* 2005;20:253-60.
28. Niimi A, Ozeki K, Ueda M, Nakayama B. A comparative study of removal torque of endosseous implants in the fibula, iliac crest and scapula of cadavers: preliminary report. *Clin Oral Implants Res* 1997;8:286-9.
29. Beer A, Gahleitner A, Holm A, Tschabitscher M, Homolka P. Correlation of insertion torques with bone mineral density from dental quantitative CT in the mandible. *Clin Oral Implants Res* 2003;14:616-20.
30. Klokkevold PR, Johnson P, Dadgostari S, Caputo A, Davies JE, Nishimura RD. Early endosseous integration enhanced by dual acid etching of titanium: a torque removal study in the rabbit. *Clin Oral Implants Res* 2001;12:350-7.

31. da Cunha HA, Francischone CE, Filho HN, de Oliveira RC. A comparison between cutting torque and resonance frequency in the assessment of primary stability and final torque capacity of standard and TiUnite single-tooth implants under immediate loading. *Int J Oral Maxillofac Implants* 2004;19:578-85.
32. Turkyilmaz I. A comparison between insertion torque and resonance frequency in the assessment of torque capacity and primary stability of Brånemark system implants. *J Oral Rehabil* 2006;33:754-9.
33. Lim SA, Cha JY, Hwang CJ. Insertion torque of orthodontic miniscrews according to changes in shape, diameter and length. *Angle Orthod* 2008;78:234-40.
34. Morarend C, Qian F, Marshall SD, Southard KA, Grosland NM, Morgan TA, et al. Effect of screw diameter on orthodontic skeletal anchorage. *Am J Orthod Dentofacial Orthop* 2009;136:224-9.
35. Mortensen MG, Buschang PH, Oliver DR, Kyung HM, Behrens RG. Stability of immediately loaded 3- and 6-mm miniscrew implants in beagle dogs--a pilot study. *Am J Orthod Dentofacial Orthop* 2009;136:251-9.
36. Simon H, Caputo AA. Removal torque of immediately loaded transitional endosseous implants in human subjects. *Int J Oral Maxillofac Implants* 2002;17:839-45.
37. Roberts WE, Smith RK, Zilberman Y, Mozsary PG, Smith RS. Osseous adaptation to continuous loading of rigid endosseous implants. *Am J Orthod* 1984;86:95-111.
38. Freire JN, Silva NR, Gil JN, Magini RS, Coelho PG. Histomorphologic and histomorphometric evaluation of immediately and early loaded mini-implants for orthodontic anchorage. *Am J Orthod Dentofacial Orthop* 2007;131:704.e1-9.
39. Meredith N, Book K, Friberg B, Jemt T, Sennerby L. Resonance frequency measurements of implant stability in vivo. A cross-sectional and longitudinal study of resonance frequency measurements on implants in the edentulous and partially dentate maxilla. *Clin Oral Implants Res* 1997;8:226-33.
40. Meredith N. Assessment of implant stability as a prognostic determinant. *Int J Prosthodont* 1998;11:491-501.
41. Veltri M, Balleri B, Goracci C, Giorgetti R, Balleri P, Ferrari M. Soft bone primary stability of 3 different miniscrews for orthodontic anchorage: a resonance frequency investigation. *Am J Orthod Dentofacial Orthop* 2009;135:642-8.
42. Meredith N, Alleyne D, Cawley P. Quantitative determination of the stability of the implant-tissue interface using resonance frequency analysis. *Clin Oral Implants Res* 1996;7:261-7.
43. Okuyama K, Abe E, Suzuki T, Tamura Y, Chiba M, Sato K. Can insertional torque predict screw loosening and related failures? An in vivo study of pedicle screw fixation augmenting posterior lumbar interbody fusion. *Spine (Phila Pa 1976)* 2000;25:858-64.
44. Ottoni JM, Oliveira ZF, Mansini R, Cabral AM. Correlation between placement torque and survival of single-tooth implants. *Int J Oral Maxillofac Implants* 2005;20:769-76.