Early bone healing onto implant surface treated by fibronectin/ oxysterol for cell adhesion/osteogenic differentiation: in vivo experimental study in dogs

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Abstract

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Purpose: This study aimed to evaluate the effects of fibronectin and oxysterol immobilized on machined-surface dental implants for the enhancement of cell attachment and osteogenic differentiation, on peri-implant bone healing in the early healing phase using an experimental model in dogs.

Materials and Methods: Five types of dental implants were installed at a healed alveolar ridge in five dogs: a machined-surface implant (MI), apatite-coated MI (AMI), fibronectin-loaded AMI (FAMI), oxysterol-loaded AMI (OAMI), and sand-blasted, large-grit, acid-etched surface implant (SLAI). A randomly selected unilateral ridge was observed for 2 weeks, and the contralateral ridge for a 4-week period. Histologic and histometric analyses were performed for the bone-to-implant contact proportion (BIC) and bone density around the dental implant surface.

Results: Different bone healing patterns were observed according to the type of implant surface 2 weeks after installation; newly formed bone continuously lined the entire surfaces in specimens of the FAMI and SLAI groups, whereas bony trabecula

from adjacent bone tissue appeared with minimal new bone lining onto the surface in the MI, AMI, and OAMI groups. Histometric results revealed a significant reduction in the BIC in MI, AMI, and OAMI compared to SLAI, but FAMI demonstrated a comparable BIC with SLAI. Although both the BIC and bone density increased from a 2- to 4-week healing period, bone density showed no significant difference among any of the experimental and control groups.

Conclusions: A fibronectin-coated implant surface designed for cell adhesion could increase contact osteogenesis in the early bone healing phase, but an oxysterol-coated implant surface designed for osteoinductivity could not modify early bone healing around implants in normal bone physiology.

Key Words: Cell adhesion, Dental implants, Fibronectins, Surface properties, Titanium.

Early bone healing onto implant surface treated by fibronectin/ oxysterol for cell adhesion/osteogenic differentiation: in vivo experimental study in dogs

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I. Introduction

Since the dental implant was first introduced, various fixture designs and surface treatments have been developed for enhancement of osseointegration (A. H. Choi et al., 2013; Sykaras et al., 2000). These designs aimed to achieve implant treatment with less time required for the healing period and longer-term clinical stability. Along the above-mentioned lines, machined-surface dental implants were replaced by those with rough surfaces (Scacchi et al., 2000). Notably, sand-blasted, large-grit, acid-etched dental implants not only provide extensively increased contact area with

adjacent alveolar bone tissue (Cochran et al., 1998), but also enhance cell attachment for *de novo* bone formation onto the implant surface (Davies, 1998).

Dental implants are supported by underlying bone tissue via direct bone contact (osseointegration); therefore, increasing the bone-to-implant contact area has been a main research topic in implant dentistry (Albrektsson et al., 1981; Weber and Fiorellini, 1992). In previous studies, newly formed bone could be observed on the dental implant surface even in fatty marrow areas (Rahal et al., 1993), in which increased bone density was observed around the dental implant compared to the marrow area. These findings can be explained by contact osteogenesis in Davies' hypothesis (Davies, 1998, 2003). The author described the mechanism of peri-implant bone healing, in which two types of healing are characterized: differential bone formation from recipient bone (distance) and attached cells onto the implant surface (contact osteogenesis). Therefore, cellular events, including attachment, proliferation, and differentiation on the dental implant surface have been suggested to be the most important factors for peri-implant bone healing and, additionally, Davies (Davies, 1998) proposed that surface topographies also affect contact osteogenesis. Many other studies have proven his hypothesis by demonstrating increased bone-implant contact around rough-surfaced implants (Cooper, 2000; Ericsson et al., 1994), such as sandblasted, large-grit, and acid-etched surfaces, compared to those with machined surfaces (Buser et al., 1999; Buser et al., 1991).

According to the theory of contact osteogenesis, the microtexture of a rough surface could retain fibrin complex on the surface, and enable enhanced attachment and migration of undifferentiated cells, which are the initial steps of bone formation (Davies, 1998; Park et al., 2001). Since the clinical success of these rough surface implants (Cochran et al., 2002; Scacchi et al., 2000), various other approaches have been developed for focusing on enhancing cellular events on the modified surfaces, that is, hydrophilic or anodized implant surfaces (Lai et al., 2010; Li et al., 2008; Qu et al., 2007; Wall et al., 2009). However, the separate effects of cellular events, such as cell attachment and differentiation, have not yet been elucidated.

The current development of implant surface technology has targeted the generation of a “biomimetic surface” on dental implants (A. H. Choi et al., 2013; Le Guehennec et al., 2007), in which biologic molecules have been applied onto the implant surface to stimulate osteogenesis and mimic each developmental step in the healing process. Extracellular matrix, peptides, and various growth factors are representative biologic molecules. Fibronectin is a major extracellular matrix that mediates attachment of cells to other cells or to other surfaces, such as the basement membrane. Recent studies have introduced a fibronectin-coated dental implant system in the research stage (Hilbig et al., 2007; Kim et al., 2011), and immobilization of fibronectin increased cell attachment (Chen et al., 2010) and osteoblastic protein expression at the *in vitro* level (Gorbahn et al., 2012). Another strategy in creating biomimetic

implant surfaces is the use of growth factors (Leknes et al., 2008; Wikesjo et al., 2008) or their natural substitutes, such as oxysterol (Son et al., 2010), for enhancement of osteogenic cell differentiation. Previous studies have demonstrated that oxysterols regulate differentiation of stem cells into osteogenic cells via the hedgehog pathway, and also prevent adipogenic differentiation *in vitro* (Aghaloo et al., 2007; Stappenbeck et al., 2012). Another *in vivo* study also found increased bone healing and augmentation in a spinal fusion model in animals (Johnson et al., 2011).

Even though these two types of biomimetic implant surface developments showed increased cell attachment and differentiation *in vitro* (Chen et al., 2010; Son et al., 2010), there was a lack of enhancement of osseointegration by using fibronectin or oxysterol in clinically-mimicking an *in vivo* animal model. Therefore, the present study aimed to evaluate the effects of fibronectin and oxysterol immobilized on machined-surface dental implants for the enhancement of cell attachment and osteogenic differentiation, on peri-implant bone healing in the early healing phase using an experimental model in dogs.

II. Materials & Methods

1. Materials

1.1 Animals

Five male mongrel dogs, aged 18–24 months and weighing approximately 30 kg, were used. All of the dogs had intact dentition and a healthy periodontium. Animal selection, management, and preparation, as well as the surgical protocol, followed the routine procedure approved by the Animal Care and Use Committee, Yonsei Medical Center, Seoul, Korea (2011-0072-1).

1.2 Implant preparation

The Machined-surface implant (MI)

Cylindrical, threaded implants of commercially pure titanium (Ø3.4 mm, 10-mm length) with a machined surface were provided from the Research Institute of Dentium, Seoul, Korea.

Apatite-coated MI (AMI)

The MI was treated by calcium phosphate (CaP) nano-coating at a thickness of 500 nm, using ion beam-assisted deposition, as described previously [22]. For apatite formation on CaP-coated surfaces, samples were immersed into the solution, including Dulbecco's phosphate-buffered saline (DPBS, Gibco-BRL, a division of

Life Technology, Grnad Island, NY, USA) and reagent grade CaCl2 (100 mg/L). Apatite-coated samples were then rinsed with distilled water twice and dried at ambient temperature.

Fibronectin-loaded and AMI (FAMI)

FAMI samples were fabricated using the same method as for AMI, except that DPBS solution containing fibronectin was used instead of normal DPBS.

Oxysterol-loaded and AMI (OAMI)

CaP-coated, MIs were immersed in DPBS solution containing oxysterol for 2 days, and washed three times with distilled water and dried. The samples were immersed again in DPBS solution without oxysterol for one more day for additional apatite coating on the oxysterol/apatite coated surface, and then washed and dried.

Sand-blasted, large-grit, acid-etched surface implant (SLAI)

Commercially available dental implants (Implantium, Dentium Co., Seoul, Korea), which were treated by large grit sand-blasting and further etching, were used as a positive control group.

2. Study design and surgical protocol

Ten experimental groups were allocated according to the type of implant surface (MI, AMI, FAMI, OAMI, and SLAI) and observational period (2 and 4 weeks). Five types of implants were installed in a randomly selected unilateral edentulous ridge, and the

same types of implants were installed on the contralateral side at 2 weeks after the first surgery. The order of installation sites was rotated in five animals for even distribution of the experimental site. After allowing differential healing periods (2 and 4 weeks) following implant installation surgery, the animals were sacrificed for histological analysis.

Twelve weeks before implant installation surgery, all premolars and first molars were extracted at both mandibles under general anesthesia and sterile conditions in an operating room using 0.05 mg/kg atropine (subcutaneous injection), 2 mg/kg xylazine (Rompun, Bayer Korea, Seoul, Korea), and 10 mg/kg ketamine hydrochloride (Ketalar, Yuhan Co., Seoul, Korea) intravenously. The dogs were placed on a heating pad, intubated, administered 2% enflurane, and monitored with an electrocardiogram. After disinfecting the surgical sites, 2% lidocaine HCl with epinephrine 1:100,000 (Kwangmyung Pharm, Seoul, Korea) was administered by infiltration at the surgical sites. Implant installation operations were also performed under the same conditions as the tooth extraction procedure. A midcrestal incision was made, and mucoperiosteal flaps were carefully reflected on the buccal and lingual aspects. The edentulous ridge was carefully flattened with a surgical bur under sterile saline irrigation in order to obtain a widened ridge to accommodate a standardized ridge shape. Five prefabricated implants were installed in rotational order from anterior to posterior sites in individual animals with an even distribution of installed sites in each

group, and the same order of installed implants was applied at both sides of the edentulous ridge in the same animal. Implant site preparation was performed by sequential drilling, and the flaps were sutured after implant installation using 5-0 resorbable suture materials (Vicryl 5/0, Polyglactin 910, Ethicon, a division of Johnson & Johnson, Somerville, NJ, USA). The sutures were removed after 7–10 days, and a soft diet was provided throughout the study period.

3. Histologic preparation

The animals were sacrificed with an anesthesia drug overdose, and block sections, including segments of implants, were preserved and fixed in 10% neutral-buffered formalin. The specimens were dehydrated in ethanol, embedded in methacrylate, and sectioned in the mesio-distal plane using a diamond saw (Exakt, Apparatebau, Norderstedt, Germany). From each implant site, a central section was taken to a final thickness of about 30 μm, and the sections were stained with hematoxylin and eosin.

4. Histologic and histometric analysis

Histologic and histometric analyses were performed using incandescent and polarized light microscopy (Olympus Research System Microscope BX51, Olympus Co., Tokyo, Japan) and a PC-based image analysis system (Image-Pro Plus, Media Cybernetic, Silver Spring, MD, USA). The bone-to-implant contact proportion (BIC)

and bone density in the space between two threads were measured along the whole length of the implants. The bone density was defined as the proportion of newly formed bone in the interthread space. At four sites among a total of 50 experimental samples, the implant apex area intruding into the mandibular canal was excluded in the histometric analysis, and this area did not exceed 2 mm in length in any of the four cases (Fig. 1).

5. Statistical analysis

One Statistical analysis was performed using a commercially avail¬able software program IBM SPSS Statistics ver. 20.0 (IBM Co., Armonk, NY, USA). The linear mixed model was used to estimate the contributions of two fixed effects (types of surface treatment and observational periods) and a random effect (animal subject) to the histometric results of the bone-to-implant interface (BIC and bone density). Because there was no interaction between the two factors (P=0.457 for BIC and P=0.359 for bone density), the experimental groups in the same observational period and the same experimental groups with different observational periods were compared separately using repeated measures analysis of variance and a paired t-test, respectively. The level of significance was set at 5%.

III. Results

1. Clinical observation

All After the use of sequential drills and a countersink drill, all implants were installed at the final torque of 30–50 N·m on the day of implant installation. All sites underwent uneventful healing during the whole experimental period, with limited signs of inflammation and cover-screw exposure.

2. Histologic observation

All specimens, except one implant, showed direct bone contact with the implant surface (osseointegration) along the whole length of the dental implants. One site in the FAMI group showed fibrous encapsulation without any bone contact, and this was excluded in histometric analyses. Four among the 50 installed implants protruded into the mandibular canal, and no bone formation occurred in the protruding area; however, those lengths did not exceed 2 or 3 threads of the dental implant from the apex.

At the observational period of 2 weeks, about half of the dental implant surfaces directly contacted the newly formed bone. Notably, in specimens from the FAMI and SLAI groups, newly formed bone continuously lined the entire surface, while the MIs with and without the other coating methods showed a partial or limited lining of osseointegration (Figs. 1 and 2). Two types of bone trabecula could be observed: One

type appeared to sprout from the recipient bone tissue (black asterisks in Fig. 2), and the other type was woven bone lining newly formed on the implant surface without any relationship with the recipient bone tissue (yellow asterisks in Fig. 2C and E). Most of FAMIs and SLAIs showed the latter type of bone tissue, suggesting contact osteogenesis in the healing processes of osseointegration.

In the specimens from all groups at 4 weeks, newly formed bone tissue increased around the surface and in the space between the implant threads (Figs. 3 and 4). The proportion of newly formed woven bone around the implant was reduced at 4 weeks compared to 2 weeks.

3. Histometric analysis

The results of histometric analyses (mean, standard deviation, and 95% confidence interval for the mean) were presented in Tables 1 and 2 and Fig. 5. Statistical analyses using a linear mixed model revealed that the BICs were significantly different between groups, according to the observational period ($P<0.01$) and type of surface treatment ($P<0.01$). At the 2-week observational period, the BIC averaged 54.08%±9.50%, 59.94%±5.49%, 68.54%± 11.42%, 58.65%±8.84%, and 77.14%±7.38% for the MI, AMI, FAMI, OAMI, and SLAI groups, respectively. The SLAI group, as a positive control, showed the highest BIC among all groups, and there were significant differences from the MI ($P<0.01$), AMI($P=0.04$), and OAMI

(P=0.03) groups. Although there was no significant difference in BIC between the FAMI and SLAI groups, the FAMI group had a wider confidence interval for the mean BIC than the SLAI group; a similar maximum level of confidence interval was found in FAMI (86.70%) and SLAI (86.30%), but the corresponding values for the minimum levels of intervals were 50.37% and 67.98%, respectively. The other experimental groups (MI, AMI, and OAMI) showed a significantly increased BIC at 4 weeks compared to the same experimental group at 2 weeks (P=0.03, P=0.04, and P=0.02, respectively). In addition, there were no significant differences in BIC between any of the groups at the 4-week observational period, when the BIC averaged 70.53%±7.77%, 71.10%±11.75%, 73.95%±9.74%, 74.94%±5.55%, and 84.34%±4.06% for the MI, AMI, FAMI, OAMI, and SLAI groups, respectively.

Significantly increased bone density was found from the 2-week to 4-week observational periods in the linear mixed model (P<0.01), but no effects were found according to the type of surface treatment (P=0.134). Bone density at the 2-week observational period averaged 29.84%±11.80%, 33.99%±4.57%, 33.78%±9.34%, 34.23%±8.99%, and 42.74%±3.42% for the MI, AMI, FAMI, OAMI, and SLAI groups, respectively. The corresponding values for bone density at 4 weeks were 46.92%±9.58%, 50.82%±11.89%, 42.62%±3.96%, 51.91%± 2.86%, and 50.18%±7.75%, respectively; there were significant differences from 2 weeks to 4 weeks in MI (P=0.02), AMI (P=0.03), and OAMI (P=0.01).

IV. Discussion

Evaluation This study was based on our two previous studies that demonstrated an increase in cell adhesion on fibronectin and apatite-coated titanium surfaces (Chen et al., 2010) and enhancement of osteoblastic differentiation by oxysterol and apatite-coated titanium surfaces (Son et al., 2010). Since the development of dental implants using titanium, various surface treatments have been studied to make a bioactive titanium surface through the concept of mimicking cellular events in bone formation and remodeling processes (A. H. Choi et al., 2013; Le Guehennec et al., 2007). The two above-mentioned types of implant surfaces were also intended to transform the surface from “biotolerant” to “bioactive” titanium: The fibronectin and apatite coating was intended to promote cellular adhesion onto the surface as a first step in the healing process (Chen et al., 2010), and the oxysterol or apatite coating was intended to promote differentiation of the adhered cells (Son et al., 2010). However, most dental clinicians still prefer rough surface implants without any biomimetic surface modification, even though various types of biomimetic surface implants have been commercially available. A systematic review of the Cochrane Collaboration reported that there was no clinical evidence of superiority in any particular type of dental implant (Esposito et al., 2007).

The present study aimed to determine whether biomimetic implant surfaces that

showed greater cell attachment and differentiation at *in vitro* level (Chen et al., 2010; Son et al., 2010) could enhance the histologic parameters of the bone-to-implant interface in experiments *in vivo* mimicking clinical situations. In the present experimental model of normal bone without any defects, two types of bone healing patterns were observed around the dental implant surface: (1) a thin rim of woven bone deposited onto the implant surface (yellow asterisks in Fig. 2); and (2) bony trabecula sprouting from recipient bone tissue and contacting the implant surface (black asterisks in Fig. 2). These correspond to distance osteogenesis and contact osteogenesis in Davies' hypothesis (Davies, 1998), respectively. In a previous study, Davies described contact osteogenesis, in which de novo bone formation occurred on the implant surface; this pattern of healing was also demonstrated in the present results (Davies, 1998, 2003). At the 2-week observational period, mineralized tissue could be seen on the implant surface contacting connective tissue fibers. Furthermore, the thickness and degrees of mineralization were varied, which indicated the bone formation process originated from the implant surface rather than the recipient bone tissue.

The sites receiving FAMI showed histologic evidence of contact osteogenesis along a larger area of the implant surface compared to the other experimental groups at 2 weeks of healing. The first step in contact osteogenesis would be cell adhesion onto the implant surface, followed by further cellular events, including proliferation and

differentiation (Park et al., 2001). Fibronectin binds to cell adhesion molecules (integrin) on the cell surface, and increases/stabilizes cell-cell/cell-stratum adhesion (Hynes, 1992; Parsons et al., 2010); therefore, these *in vivo* results might be caused by the function of fibronectin, like *in vitro* results. This healing pattern could also be demonstrated in sites receiving SLAI as a positive control group. Numerous previous studies have already found increased bone-to-implant contact in SLA-surfaced implants compared to MIs, which resulted from increased surface energy by microroughness of the surface (Abrahamsson et al., 2004; Buser et al., 1991; Piattelli et al., 1998). In the histometric results, the SLAI group showed a higher BIC compared to the other three experimental groups (MI, AMI, and OAMI), and there was no significant difference between the FAMI and SLAI groups. However, the FAMI group also did not show any differences from the other groups, unlike the SLAI group. While the SLAI group showed a narrow range of histometric results, sites receiving FAMI showed a relatively wide range of results with regard to the BIC proportion; 95% confidence intervals for the mean were 67.98–86.30 in the SLAI group and 50.37–86.70 in the FAMI group. Rough surface implants can provide increased contact surface and mechanical interlocking with the recipient bone tissue (Cooper, 2000; Li et al., 2002), and these might increase the stability of SLAI during the early healing period. Increasing the stability of implants could also stabilize the *in vivo* healing process, which can be influenced by not only cellular events, but also the

various environments of the recipient site (bone quality, biologic responses by cytokines, and immune responses). For this reason, FAMI might show a less uniform increase in the BIC compared to the SLAI, despite enhancement of cell adhesion.

Oxysterol is an oxidized derivative of cholesterol, and its novel characteristic of regulating differentiation into osteogenic cells has been the subject of increasing research attention. In previous studies, oxysterol induced *in vivo* osteogenesis like bone morphogenetic protein-2 (BMP-2), or synergistically increased the osteoinductive effects of BMP-2 (Amantea et al., 2008; Johnson et al., 2011; Kha et al., 2004). Since complications of BMP-2 application have emerged in research and clinical fields (Y. Choi et al., 2013; Zara et al., 2011), oxysterol has received attention as a substitute or regulating factor for BMP-2. Our previous study also showed an increase in alkaline phosphatase with oxysterol surface coating, and simultaneous apatite and oxysterol coating could synergistically enhance *in vitro* osteogenesis (Son et al., 2010). In the present study, the authors hypothesized that osteoinduction by oxysterol could enhance bone formation by osteoblasts adhered to the implant surface, and increase the BIC and bone density in the early healing phase. However, oxysterol coating on the implant surface failed to enhance the BIC and bone density in the space between threads, and these findings are in agreement with a previous study (Wikesjo et al., 2008) that demonstrated that implant surface coating with recombinant human BMP-2 did not increase the BIC or bone density in a nondefect,

normal bone area, despite successful vertical augmentation in the supra-alveolar defect area without any graft materials (Leknes et al., 2008; Wikesjo et al., 2008). Osteoinductive molecules might not accelerate or enhance bone healing at the bone-to-implant interface in normal bone, even though they can increase bone formation in the area with unfavorable defects. However, to confirm these hypotheses, further studies should be performed in various defect models.

This study aimed to determine the effects of enhancement of cell adhesion onto the implant surface and osteogenic differentiation by surface coating techniques on bone healing processes, especially at the bone-to-implant interface, in the early healing phase. Two types of implants focusing on cell adhesion increased the BIC at 2 weeks after implant installation: sand-blasted/acid-etched and fibronectin-coated surface implants. However, surface coating with osteoinductive molecules did not modify the BIC or bone density around any of the implant surfaces. Cell adhesion onto the implant surface may enhance contact osteogenesis around the implant in the early healing phase, when the implant is installed in normal bone without any defect.

V. Conclusions

A fibronectin-coated implant surface designed for cell adhesion could increase contact osteogenesis in the early bone healing phase, but an oxysterol-coated implant surface designed for osteoinductivity could not modify early bone healing around implants in normal bone physiology the limits of this study,

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Legends

Figure 1. Representative photomicrographs of all experimental and control groups at 2 weeks after implant installation. All specimens showed initial bony healing phases around dental implants, in which woven bone could be found at the prepared or resorbed area of the recipient alveolar bone. An increased number of thin bony trabeculae in newly formed bone was demonstrated in the area adjacent to the implant, including the spaces between threads. There were no significant differences between groups visible at this low magnification. Some implants (4 of a total of 50 experimentally installed implants) protruded into the mandibular canal, due to a lack of height of the residual alveolar ridge (C; arrows indicate superior border of the mandibular canal). These pieces of implant in the canal area were excluded from the histometric analyses. (A) Machined-surface implant (MI), (B) apatite-coated MI (AMI), (C) fibronectin-loaded and AMI, (D) oxysterol-loaded and AMI, and (E) sand-blasted, large-grit, and acid-etched surface implant. The scale bars in all panels were 1 mm.

Figure 2. High magnification views of representative experimental and control

samples at 2 weeks. All photographs were taken from the middle of the implants, showing the space between the implant threads. In these spaces of machined-surface implant (MI) (A), apatite-coated MI (AMI) (B), and oxysterol-loaded and AMI (D), thin bony trabecula that appeared sprouting from the recipient bone (black asterisks), approached the implant surfaces, whereas fibronectin-loaded and AMI (C) and sand-blasted, large-grit, and acid-etched surface implant (E) showed rims of newly formed bone contacting the implant surface (yellow asterisks) in most of the surface area, indicating contact osteogenesis. The scale bars in all panels represent 100 μm.

Figure 3. Representative photomicrographs of all experimental and control groups at 4 weeks after implant installation. The woven bone area had decreased in all of the specimens at the 4-week observational period. Most of the spaces between threads were filled with lamellated bone rather than woven bone, and increased, direct contact of bone to dental implants could be found along the whole length of the dental implants. There were still no significant differences in bone healing visible at the bone-to-implant interface in low magnification views. (A) Machined-surface implant (MI), (B) apatite-coated MI (AMI), (C) fibronectin-loaded and AMI, (D)

oxysterol-loaded and AMI, and (E) sand-blasted, large-grit, and acid-etched surface implant. The scale bars in all panels represented 1 mm.

Figure 4. High magnification views of representative experimental and control samples at 4 weeks. All of the spaces between threads were filled with newly formed bone with high density. (A, B, D) Newly formed bone appeared in these spaces, approaching the implant surface from the recipient bone. The newly formed bone was partially in contact with the surface. (C, E) Thickened rims of newly formed bone on the surface could be found at most of the installed implant surface area, and connected with recipient bone tissues or regenerated bone sprouting from the lamellated bone around the dental implants. (A) Machined-surface implant (MI), (B) apatite-coated MI (AMI), (C) fibronectin-loaded and AMI, (D) oxysterol-loaded and AMI, and (E) sand-blasted, large-grit, and acid-etched surface implant. Scale bars in all panels were 100 μm

Figure 5. Results of histometric analyses of the proportion of bone-to-implant contact (%) and bone density (%). Asterisks (*) indicate significant differences as shown by statistical analyses. MI: machined-surface implant, AMI: apatite-coated MI, FAMI: fibronectin-loaded and AMI, OAMI: oxysterol-

loaded and AMI, SLAI: sand-blasted, large-grit, and acid-etched surface implant.

Tables

Table 1 Results of histometric analyses in bone-to-implant contact proportion.

(SD: standard deviation, CI: confidence interval, MI: machined-surface implant, AMI: apatite-coated MI, FAMI: fibronectin-loaded and AMI, OAMI: oxysterol-loaded and AMI, SLAI: sand-blasted, large-grit, and acid-etched surface implant.).

Group	2 weeks		4 weeks	
	Mean±SD	95% CI	Mean±SD	95% CI
MI	54.08±9.50*	42.29–65.88	70.53±7.77§	60.88–80.17
AMI	59.94±5.49†	52.72–66.36	71.10±11.75§	56.51–85.69
FAMI	68.54±11.42	50.37–86.70	73.95±9.74	61.86–86.04
OAMI	58.65±8.84‡	47.66–69.63	74.94±5.55§	68.04–81.83
SLAI	77.14±7.38	67.98–86.30	84.34±4.06	79.30–89.38

* : Significantly different between measurements in MI and SLAI groups (P=0.004).

† : Significantly different between measurements in AMI and SLAI groups (P=0.031).

‡ : Significantly different between measurements in OAMI and SLAI groups (P=0.022).

§ : Significantly different between at 2- and 4-week period measurements in the same group (d)P=0.019,e)P=0.042, f)P=0.015)

Table 2 Results of histometric analyses in bone density

(SD: standard deviation, CI: confidence interval, MI: machined-surface implant, AMI: apatite-coated MI, FAMI: fibronectin-loaded and AMI, OAMI: oxysterol-loaded and AMI, SLAI: sand-blasted, large-grit, and acid-etched surface implant.)

Group	2 weeks		4 weeks	
	Mean±SD	95% CI	Mean±SD	95% CI
MI	29.84±11.80	15.18–44.50	46.92±9.58 ‖	35.02–58.82
AMI	33.99±4.57	28.31–39.67	50.82±11.89 ‖	36.06–65.58
FAMI	33.78±9.34	18.91–48.65	42.62±3.96	37.71–47.53
OAMI	34.23±8.99	23.07–45.39	51.91±2.86 ‖	48.36–55.46
SLAI	42.74±3.42	38.49–46.98	50.18±7.75	40.55–59.80

‖ : Significantly different between at 2- and 4-week period measurements in the same group (a) P=0.014, b) P=0.017, c) P=0.010).

Figures

Figure 1

Figure 2

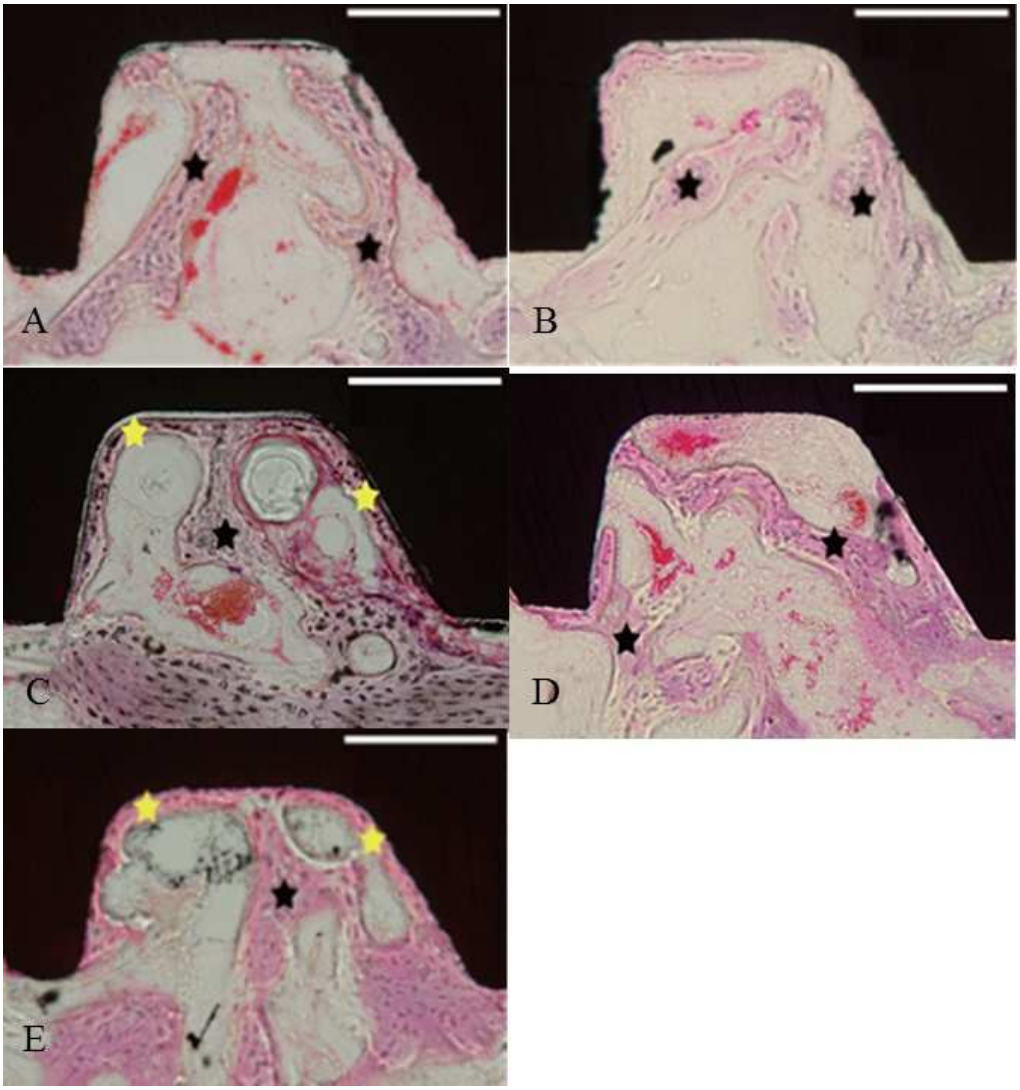


Figure 3

Figure 4

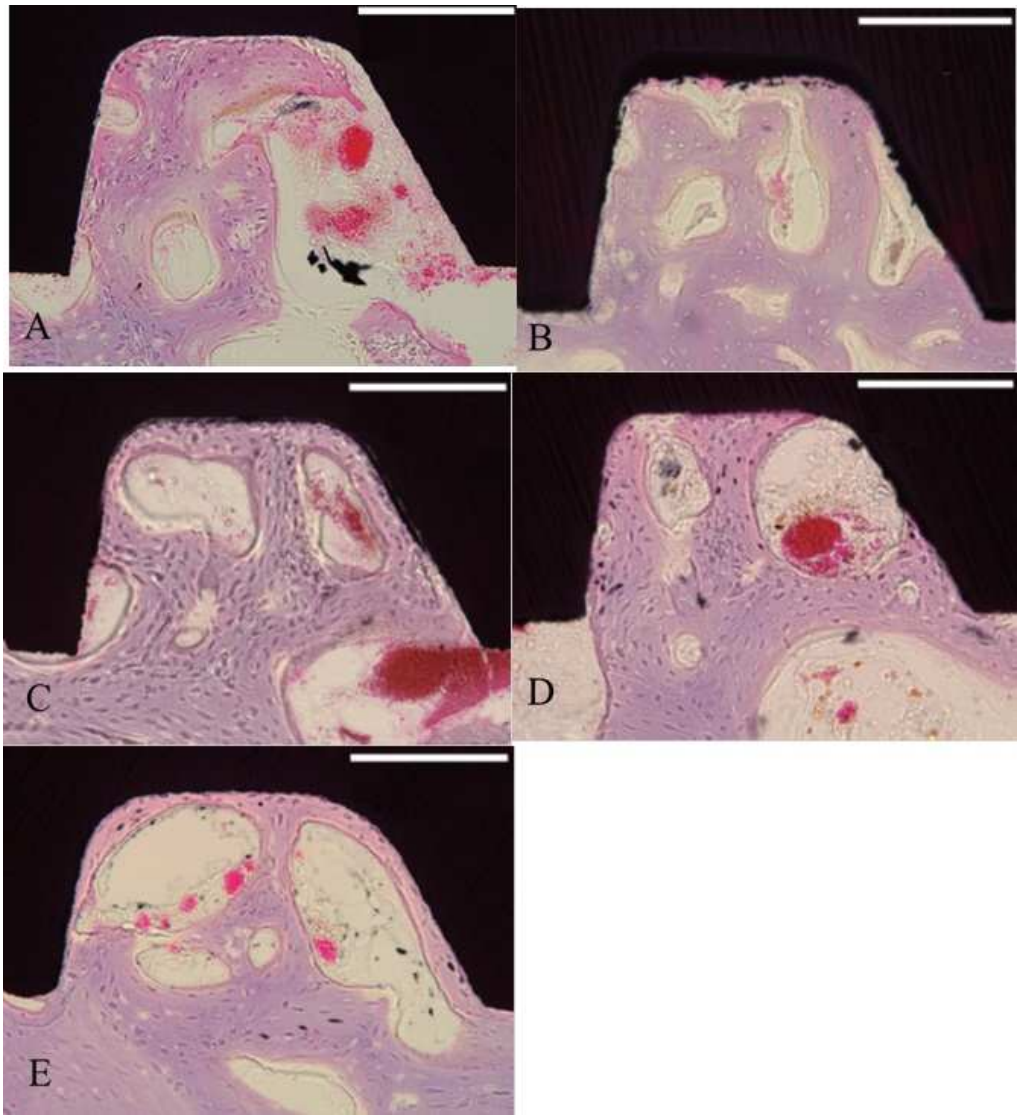
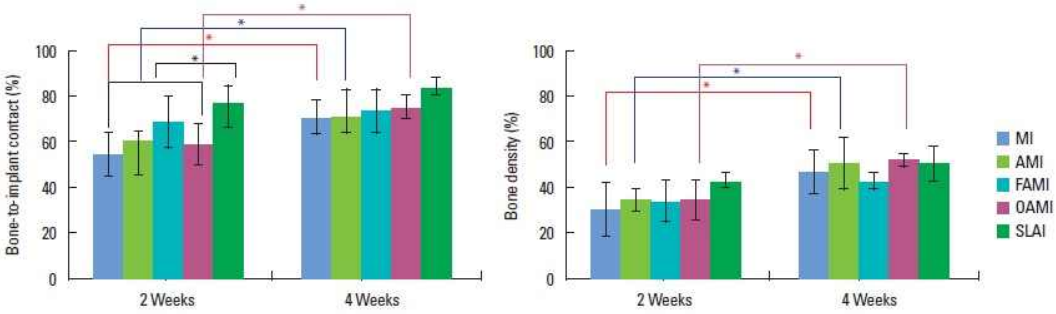


Figure 5



국문요약

성견에서 파이브로넥틴/옥시스테롤로 표면처리한 임플란트의 세포부착과 골분화에 의한 초기 골치유에 대한 연구

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양 진 혁

골분화와 골유도에 탁월함이 입증된 파이브로넥틴과 옥시스테롤로 표면처리한 치과용 임플란트를 성견모델에서 식립하여 임플란트 주변에서의 세포부착과 골분화에 의한 초기 치유과정을 평가함이 이번 연구의 목적이다.

5종류로 표면처리한 임플란트를 5마리 성견의 발치 후 치유된 치조골에 식립하였다. 임플란트의 표면처리는 다음과 같다; 무처리한 표면의 임플란트 (MI-machined-surfaced implant), 아파타이트로 코팅한 임플란트 (AMI-apitite-coated implant), 파이브로넥틴으로 코팅한 AMI (FAMI-fibronectin-loaded AMI), 옥시스테롤로 코팅한 AMI (OAMI-oxysterol-loaded AMI), SLA 임플란트 (SLAI-sand-blasted, large-grit, acid-etched surface implant). 무작위로 선택된 편측의 치조골에서

임플란트를 식립한 후에 2, 4주의 치유기간 후 임플란트가 제거되었고 희생시켜 조직 계측학적 분석을 위한 시편을 제작하였다. 조직학적과 조직계측학적 분석은 골-임플란트 접촉 비율 (BIC- bone-to-implant contact proportion)과 임플란트 표면의 골밀도 (bone densitiy)를 계측했다.

2주 치유에서는 임플란트 표면의 종류에 따라 다른 형태의 골치유 양상을 보였다. FAMI군과 대조군인 SLAI군에서는 임플란트 표면에서 연속적으로 나열된 신생골을 관찰할 수 있었다. 반면에, MI, AMI, OAMI 군들에서는 임플란트 표면에서는 미약한 신생골을 형성과 주변골로부터 나온 골소주를 관찰할 수 있었다. 조직계측학적 평가 연구에서는 대조군인 SLAI 군에 비해 MI, AMI, OAMI 군들에서 BIC값이 현저히 낮았으나, FAMI군은 대조군과 유사한 값을 보였다. 2주와 4주 치유 비교연구에서는 모든 군에서 시간이 지남에 따라 골-임플란트 접촉 비율(BIC- bone-to-implant contact proportion)과 임플란트 표면의 골밀도 (bone densitiy)는 증가한 결과를 보였으나, 골밀도는 실험군과 대조군들 사이의 유의한 차이를 보이지 않았다.

세포 부착을 위해 고안된 파이브로넥틴으로 코팅처리한 임플란트는 초기 골 치유 양상에서 골접촉성 골형성 (contact osteogenesis)을 보였으나 골유도작용을 위해 고안된 옥시스테롤로 코팅처리한 임플란트는 일반적인 골 환경에서의 초기양상에는 어떠한 변화를 보여주지 못한다.

핵심되는 말: 세포부착, 치과용 임플란트, 파이브로넥틴, 표면성질, 티타늄