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Cardiac Implantable Electronic Devices and Magnetic Resonance Imaging

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Magnetic resonance imaging (MRI) is an excellent body imaging modality. One limitation of MRI is that the physical environment may be a risk for patients with implantable metallic devices. In the past, a cardiac implantable electronic device (CIED) was an absolute MRI contraindication. However, since the introduction of MRI-conditional CIED, the indication for MRI examination has progressed significantly. Cardiac magnetic resonance (CMR) examination can also be performed restrictively in patients with MRI-conditional CIED. With the physical MRI environment, the CIED located near the heart can impact especially a CMR examination focused on the heart. Furthermore, in basis of the physical MRI environment, CMR techniques have been designed for the visualization of a continuously beating heart with minimal image artifact. Therefore, physicians should be familiar with prerequisite conditions for a safe CMR, and prepare the CMR protocol to minimize CIED-related artifacts on CMR images.

 Key words
 Heart · Magnetic resonance imaging · Cardiac pacemaker, artificial · Cardiac resynchronization therapy devices · Cardioveter-defibrillators, implantable.

INTRODUCTION

Magnetic resonance imaging (MRI) is an invaluable modality for body imaging that uses a powerful static magnetic field, rapid gradient switching, and radiofrequency (RF) pulses [1]. Cardiac magnetic resonance (CMR) examination has rapidly increased in use and application as a novel hardware, software, and processing technique [2]. Thus, CMR imaging has become a valuable tool for non-invasive heart disease detection and characterization [2-5]. Cardiac implantable electronic device (CIED) generally refers to implanted cardiac pacing devices, such as the cardiac pacemaker (PM), implantable cardioverter defibrillator (ICD), and cardiac resynchronization therapy (CRT) [6-8]. The CIED consists of complex electronic and ferromagnetic components that can physically interact with the MRI environment [6,8]. Thus, CIED may be harmful to patients because of unmalfunction during an MRI examination [6,8]. Furthermore, CIED ferromagnetic components may produce susceptibility artifacts or signal void during MRI [9,10]. Therefore, CIED has conventionally been regarded as an obstacle to both the safety and image quality of CMR examination. There is a high likelihood that patients with CIED will need MRI examinations over the lifetime of their CIED [11,12]. Due to recent technical developments clinical reports have indicated that MRI can be performed safely under certain specific and controlled conditions, even in patients with CIED [7,8]. CMR may be necessary for diagnosing underlying cardiomyopathy, evaluating arrhythmogenic substrates, and disease progression assessment [3,4,13]. The risk to benefit ratio may be significantly affected by the safety and image quality of CMR examination in the CIED setting [8,14]. Thus, when considering the clinical role of CMR in patients with CIED, knowledge of CIED and MRI physics should be obtained to ensure a safe CMR examination. This review provides basic information about clinical considerations and pre-

predictable physical movement, potential for burns, or CIED

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requisites for CMR imaging in patients with CIED.

CIED COMPONENTS AND CLINICAL ROLES

CIED main components are as follows: pulse generator, leads and electrodes (Fig. 1) [8,15]. The CIED pulse generator is placed on the chest wall under the skin, and consists primarily of the battery and capacitors. The electrode is the non-insulated segment of the wire used to detect cardiac arrhythmia, pacing and provide shock stimulation to the heart. CIED electrodes typically enter via the cardiac trabeculae or screw into the myocardium. The right atrial appendage, the apex of the right ventricle, and cardiac veins along the lateral wall of the left ventricle are preferred electrode implant sites. The size, component, and position of CIED may influence adverse event and image quality in CMR imaging [14,16]. Chest radiography is a useful imaging modality for evaluating CIED physical characteristics [9,17]. Before a CMR scan, chest radiography can be used to predict the interaction between CMR imaging and CIED.

CIED systems, including the cardiac PM, ICD, and CRT have been used to correct abnormal heart rhythm in cardiovascular diseases (Table 1) [6,8]. The cardiac PM is an electronic device that causes cardiac contraction during periods of bradycardia



Fig. 1. Components of cardiac pacemaker (PM) and implantable cardioverter defibrillator (ICD). (A) Frontal chest radiography shows a pulse generator (white arrow) and right heart chamber PM leads. (B) Radiography shows the PM pulse generator, including battery. (C) ICD includes the pulse generator, leads, and right ventricular shock coil that appears as a thick band (black arrow). (D) Lateral chest radiography shows a right ventricular lead (black arrow) and a right atrial lead (white arrow) of PM.

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using small electrical stimuli [18]. Cardiac PM has been used for the management of congestive heart failure combined with ventricular dyssynchrony. The ICD is a battery-powered device for generating a large amount of electrical energy used to defibrillate the heart [8]. The clinical purpose of ICD is to terminate a life-threatening ventricular arrhythmia and prevent sudden cardiac death [18]. The main components of an ICD are a pulse generator and leads that use a right ventricular short coil as a ring electrode. The ICD has a high-voltage coil electrode which appears as a thick band on chest radiography [15]. The CRT device is a special cardiac PM that specifically aims to improve effective coordination of cardiac systole [18]. The CRT also consists of a pulse generator and leads that enable both ventricles of the heart to be stimulated at the same time. The CRT can improve heart function, reducing the symptoms of heart failure by adjusting the timing of the heart's systoles [18].

CIED safety in the MRI environment

Research results have indicated that although many patients with CIED have been reluctant to undergo MRI examinations,

 Table 1. Cardiac implantable electronic device indications

Cardiac pacemaker

- Symptomatic sinus bradycardia (<40 beats/min)

- Complete atrioventricular (AV) block

- First- or second degree AV block with hemodynamic compromise Implantable cardioverter defibrillator

- Medically refractory symptom with hypertrophic cardiomyopathy

- Congestive heart failure

- Ventricular mechanical dyssynchroncy

Cardiac resynchronization therapy-biventricular pacemaker

- QRS duration of >120 ms

- Left ventricular ejection fraction <35%

- Drug-refractory congestive heart failure

hazardous or fatal outcomes have only occurred in a small number of patients [7,17]. CIED-related hazards in MRI scanning generally arise from 3 risk sources: the static magnetic field, gradient magnetic fields, and RF pulses [19]. These risk sources may cause mechanical pull, heating, torque, vibration, and electrical stimulation. The threat of mechanical pull increases with the magnetic field strength, which is related to the amount of ferromagnetic materials in the CIED [7]. CIEDs have been found to be safe beyond the first 6 weeks following implantation because healing around the CIED acts as adequate anchorage [7,8]. In the CIED pulse generator, a reed switch has been used to activate the CIED magnet mode [17]. When the electromagnetic effect is activated, dysfunction of the reed switch can cause abnormal voltage in a sensing amplifier, triggering a circuit that controls the magnet mode functional status which can be hazardous for patients with CIED [17,20]. The MRI pulsed gradient, in addition to RF pulses, can induce electric currents in the CIED leads and electrodes. Furthermore, ICD shock delivery in the MRI environment may be disabled by the external magnetic field [17,20]. The RF energy from an imaging sequence is nonionizing electromagnetic radiation with a high frequency range [17,20]. Recurrent RF pulses can induce strong RF energy deposition and tissue damage with particularly intense local heating [17,20]. The local thermal effect from RF pulses might eventually cause an increase in pacing threshold, capture loss, or arrhythmic attack [17,20].

MRI-conditional CIED

CIED manufacturers have invested in developing both CIED hardware and software that will perform reliably during MRI scanning (Table 2). The United States Food and Drug Administration (US-FDA) has established the following categories: 1) "MRI safe", 2) "MRI-conditional", and 3) "MRI unsafe". MRI safe indicates an item that poses no known hazards in all MRI en-

Company	Device	Model	Approved range
Biotronik	Pacemaker	EVIA DR-T	3Т
	Pacemaker	EVIA SR-T	3T
	Pacemaker	SAFIO S	3Т
	Pacemaker	SOLIA S, T, JT	3Т
	ICD	IFORIA 7 DR-T	1.5T
	ICD	IFORIA 7 VR-T	1.5T
Boston Scientific	Pacemaker	Accolade MRI SR	3Т
	Pacemaker	Accolade MRI DR	3Т
	Pacemaker	Ingevity MRI lead	3Т
	Pacemaker	Fineline Lead	1.5T
	ICD	Autogen MRI SR	1.5T
	CRT	Acuityx4	1.5T

Table 2. Commercial MRI conditional cardiac implantable electronic device introduced in 2016: cardiac pacemaker, ICD, and CRT

MRI: magnetic resonance imaging, ICD: implantable cardioverter defibrillator, CRT: cardiac resynchronization therapy

vironments [8,21]. MRI-conditional suggests a device that has no known hazard in a specified MRI environment, with specified conditions for use [8,21]. The first MRI-conditional PM system was introduced in Europe by Biotronik (Berlin, Germany) in 2010, and US-FDA approved the clinical use of Medtronic's MRI-conditional PM (Minneapolis, MN, USA) in January 2011 [7]. Hardware alterations in MRI-conditional CIED include minimization of ferromagnetic materials, specific filters to prevent over- and under-sensing, resonant frequency lead, and replacement of the Reed switch [17]. Although MRI examination can be performed in patients with MRI-conditional cardiac PM using 1.5T and 3T MRI systems, a strong magnetic field strength (3T) can cause higher electromagnetic interference and local specific absorption rate (SAR), especially in an ICD that has a large battery-powered device. MRI-conditional CIED software also changes to prevent abnormal pacing during MRI scan-

Table 3. MRI recommendations for patients with a CIED

Before MRI examination

- Identify the MRI-conditional components
- MRI-conditional CIED specifications
- CIED body location
- CIED implant date (>6 weeks after implantation)
- No broken or fracture CIED leads

Program the CIED to the appropriate MRI mode

During MRI examination

Limit the static magnetic field strength to 1.5T, if possible Limit the specific absorption rate to less than 2 W/kg of body weight

Limit maximum gradient slew rate to 200T/m/s.

Minimize the number and length of sequences.

After MRI examination

Assess for new CIED-associated abnormalities that might have developed

Reprogram to the original CIED setting

MRI: magnetic resonance imaging, CIED: cardiac implantable electronic device



ning [17]. In addition, MRI protocols should be provided in the device manufacturer specifications. The use of MRI-conditional CIED is a prerequisite for CMR imaging in patients with CIED. Furthermore, the approved CMR imaging protocol can be limited by MRI system and CIED type parameters. If possible, most CIED manufacturers recommend a maximum static magnetic field strength of 1.5T, with a maximum specific SAR value of 2 W/kg for each sequence, and a maximum gradient slew rate of 200T/m/s [17]. Monitoring and resuscitation equipment must also be available during MRI examination [17]. Thus, patients with MRI-conditional CIED systems might undergo CMR scanning with minimal risks, when well-defined imaging and monitoring protocols are established (Table 3).

Magnetic susceptibility artifact on MRI

Magnetic susceptibility is the ability of a substance to become magnetized [1,22]. Heterogeneous magnetization in the target tissue of interest results in a difference in processional frequency and phase [1,22]. This causes signal loss and dephasing at the target tissue interface. Ferromagnetic objects have a very high magnetic susceptibility and can distort images, which is more prominent in gradient echo sequences. In patients with CIED, the main cause of susceptibility artifact is the CIED ferromagnetic pulse generator within the CMR imaging volume. The following recommendations can help minimize susceptibility artifact: 1) adjust the MRI scan range to avoid the artifact, 2) use a spin echo sequence instead of gradient echo, and 3) use a short echo time (TE) with a broad bandwidth to minimize dephasing [1,16,22]. The CIED can interfere with the diagnostic value of CMR imaging because the CIED ferromagnetic components have magnetic susceptibilities that are very different from human tissue.

CIED-related artifact in CMR imaging

The extent of CIED-induced artifact is mostly affected by the CIED pulse generator, and CMR protocol [16]. The CIED lead



Fig. 2. Using 3T magnetic resonance (MR) system, comparison of cardiac MR (CMR) artifacts (arrows) caused by the pacemaker on (A) T2-weighted CMR; (B) perfusion CMR; (C) cine CMR; (D) late gadolinium enhancement (LGE) CMR; and (E) T1 map CMR images.

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does not typically compromise diagnostic CMR image quality. Artifacts caused by CIED leads did not affect image interpretation in any patient, regardless of CMR sequences [16]. The size and orientation of the artifact were associated with the direction and strength of the magnetic field, the relative magnetic susceptibility of CIED, and CMR sequences (Fig. 2). Steady-state free precession (SSFP) gradient echo and inversion recovery sequences with long TE are associated with more remarkable susceptibility artifacts than are the gradient-recalled-echo (GRE) and spin echo sequences. The CMR protocol generally consists of T2weighted, perfusion, cine, late gadolinium enhancement (LGE) CMR images, and a T1 CMR map. CM images are typically viewed with: two-chamber view (2CV), four-chamber view (4CV), and short axis view (SAV). On cine CMR images (Fig. 3), artifacts are more pronounced in the SAV than in the 2CV and 4CV because of the proximity between the CIED generator and affected regions of the heart in each view [16,23]. On LGE-CMR images (Fig. 4), artifacts are most often localized to the anterior and apical myocardial segment of the left ventricle [16,23]. This artifact can significantly impact the LGE-CMR compared with T2-weighted, and perfusion CMR images [16,23]. T2-weighted images scanned by the turbo spin echo sequence show fewer susceptibility artifacts [16,23]. Myocardial T1 CMR maps also have weak susceptibility for artifacts because the T1 CMR map is based on the SSFP sequence [5]. CMR protocol modifications have been suggested to minimize CEID-related artifact in CMR



Fig. 3. Cardiac pacemaker (PM) artifacts on 3T cine cardiac magnetic resonance (CMR) images using steady-state free precession sequence. (A) The two-chamber view of cine CMR image shows a large artifact (arrow) from the PM pulse generator. (B) The four-chamber view of cine CMR image shows artifact (arrow) from the PM lead. (C) The short-axis cine CMR image shows a large cardiac PM-related artifact (arrow) that interrupts identification of the left ventricle.



Fig. 4. Cardiac pacemaker (PM) artifacts on sequential short-axis images of 3T late gadolinium enhancement (LGE) cardiac magnetic resonance (CMR) images. Sequential short-axis LGE-CMR images show the large pulse generator artifacts of cardiac PM (white arrow) obscuring the anterior segments of apical and mid-left ventricle, and the limited artifact (black arrow) from PM lead in the right ventricular chamber.

Table 4. Minimization strategies for CMR image artifact from a CIED

Prerequisite conditions and protocol for CMR imaging in patients with CIED

Long distance (>6 cm) between the CIED pulse generator and heart

Right chest CIED pulse generator

Long-axis plane of CMR scan rather than short-axis plane

Short-axis plane of CMR scan at the basal left ventricle

Frequency scout prior to SSFP

Adjusting the center offset frequency to transfer artifact using SSFP sequence

Spoiled GRE sequence with wide bandwidth rather than SSFP

MRI: magnetic resonance imaging, SSFP: steady-state free precession, GRE: gradient-recalled-echo, CMR: cardiac magnetic resonance, CIED: cardiac implantable electronic device



Fig. 5. The cardiac pacemaker (PM)-related artifacts on different 3T late gadolinium enhancement (LGE) cardiac magnetic resonance (CMR) imaging views. (A) The short axis view of the LGE-CMR image reveals the entire basal left ventricular wall completely, and shows little artifact from the PM lead in the right ventricular chamber. (B) The two-chamber view of the LGE-CMR image shows a large artifact from a cardiac PM pulse generator (arrow) in the mid- and apical left ventricle. (C) The four-chamber view of LGE-CMR image shows no remarkable artifact.

images (Table 4). The 4CV of the CMR examination can describe the entire appearance of the heart with little artifact (Fig. 5). The SAV plane of the CMR examination can be used to evaluate the basal left ventricle in patients with CIED. Changing the center offset frequency can help transfer dark-band artifacts away from the region of interest using SSFP sequence [24]. The GRE sequence and wide bandwidth can provide higher image quality and minimize artifacts in the CMR imaging [16].

CONCLUSION

Both CIED system and CMR imaging have become increasingly important in cardiac disease management. The high probability of cardiovascular disease has increased the need for CMR imaging, even in patients with CIED. Although the MRI-conditional CIED has provided opportunity for CMR imaging, safety is not absolutely guaranteed. Furthermore, the image artifact from CIED can compromise the interpretability of CMR images. Appropriate protocols that address safety and optimize CMR imaging diagnostic quality are necessary in patients with MRI-conditional CIED.

Conflicts of Interest .

The authors declare that they have no conflict of interest.

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