

2003 6





	ii
	1
I.	3
II.	5
1.	5
가.	5
.	5
2.	5
3.	6
4.	6
III.	8
1.	8
2.	5mm	8
3.	11mm	8
4.	15mm	9
IV.	16
V.	21
	22
	26

1. Piezolith 2501	7
2.	11
3.	12
4.	13
5.	
	15
6.	
	15
1.	14

(p>0.05) 가

가 (p<0.0001) 가

가 50

, 130 가

가

가 ,

50

: , , ,

< >

I.

1982

1

가

가

.

가

가

2,3

(energy)

()

(frequency;

()

가

)

가

.⁴⁻⁶

가

가

가

,⁷⁻⁹

.^{4,5}

Dornier HM3 (Dornier

Medical System, Munich, Germany)

가

60-80

2, 3

(nonsynchronous shock wave)

10-12

90-120

.^{13,14}

가

가

가

.

75 150 가 300 600 Vallancien¹⁵ 가
 가 , Wiksell Kinn¹⁶ 2
 (30) 0.4 (150)
 , Weir¹⁷ 60,
 80 117 80 117 가 가
 가 . Robert¹⁸ 240
 60
 가 가
 가
 가

II.

1.

가.

가 (: 5mm, : 5mm, 11mm, 15mm) Wolf 「Piezolith 2501」
5mm $0.130 \pm 0.005\text{gm}$, 11mm
 $0.260 \pm 0.005\text{gm}$, 15mm $0.350 \pm 0.005\text{gm}$
가
30 가

가

35mm, 6mm, 1mm

2.

(piezoelectric type) Wolf 「Piezolith 2501」
(positive pulse duration)
1 μsec (rise time) 30nsec
가 11mm
50-150MPa
가
500
90 가 50MPa 가

150MPa 가
 가
 100MPa . 5mm 500
 400
 400 .

3.

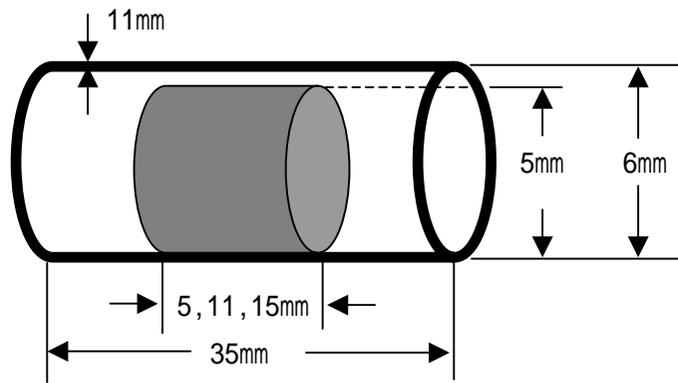
가
 (1.A)
 「Piezolith 2501」
 (1.B). 가
 11mm 15mm 500 5 mm
 400 . 가
 100MPa . 30, 50, 70, 90, 110,
 130, 150 6
 . 가 가

가 2mm
 2) (petri dish) , 40°C 30 (

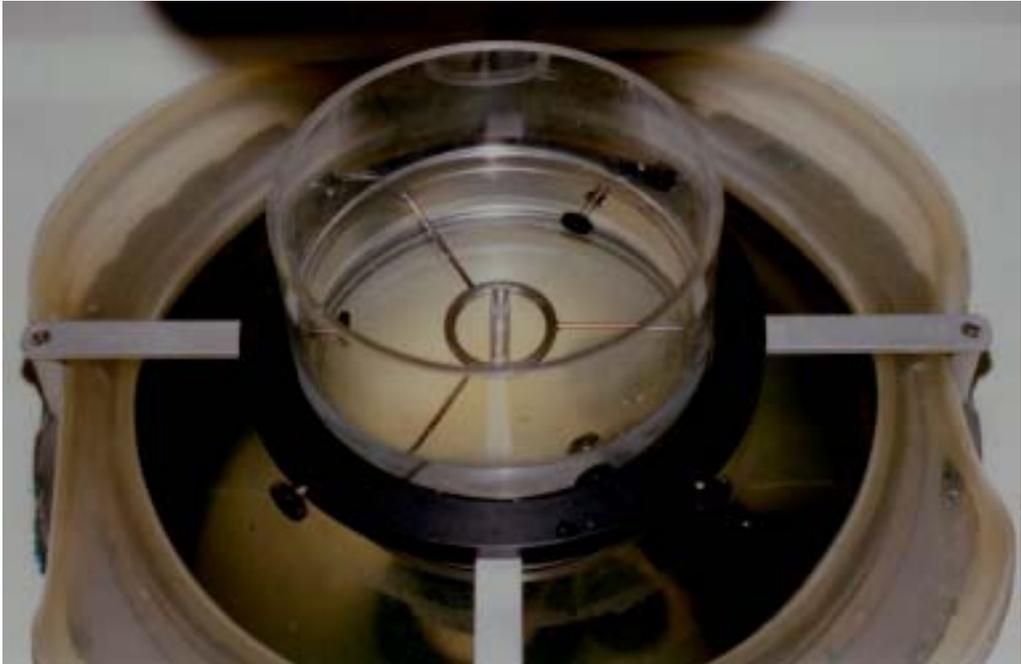
4.

2mm
 ,
 one-way ANOVA test ,
 p 0.05 가 .

A.



B.



1. Piezolith 2501

. A.

. B. 「Piezolith 2501

」

가 0.260 ± 0.005gm
 가 2mm 가
 30 21.2 ± 3.0 , 50 18.3 ± 3.3 , 70 12.8 ±
 3.5 , 90 13.7 ± 2.3 , 110 12.5 ± 2.5 , 130
 11.2 ± 2.2 , 150 9.0 ± 2.7 , p 0.0001
 가 (p < 0.05;
 1). 가 30 0.112 ±
 0.013gm, 50 0.115 ± 0.018gm, 70 0.118 ± 0.021gm, 90
 0.110 ± 0.020gm, 110 0.108 ± 0.017gm, 130
 0.110 ± 0.017gm, 150 0.102 ± 0.012gm , p
 0.7739 가
 (p > 0.05; 1). 가 30 50
 2x2mm 3x3mm가 130
 150 4x5mm 5x5mm (
 4.A). 5 6

4. 15mm

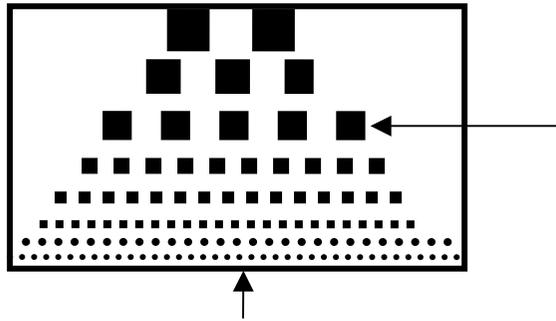
가 0.350 ± 0.005gm
 가 2mm 가 30
 24.5 ± 6.3 , 50 21.3 ± 3.2 , 70 17.0 ± 2.8 ,
 90 14.5 ± 2.3 , 110 15.7 ± 1.9 , 130 11.7
 ± 4.5 , 150 12.5 ± 3.1 , p 0.0001
 가 (p < 0.05; 1).
 가 30 0.187 ± 0.018gm,
 50 0.182 ± 0.021gm, 70 0.177 ± 0.016gm, 90
 0.172 ± 0.024gm, 110 0.188 ± 0.022gm, 130 0.167 ±
 0.025gm, 150 0.198 ± 0.024gm , p 0.2213
 가
 (p > 0.05; 1). 가 30 50

2x3mm 3x3mm가 130
150 4x5mm 5x5mm (2,
4.B). 5 6



2. . 15mm 130
500 가
()

A.



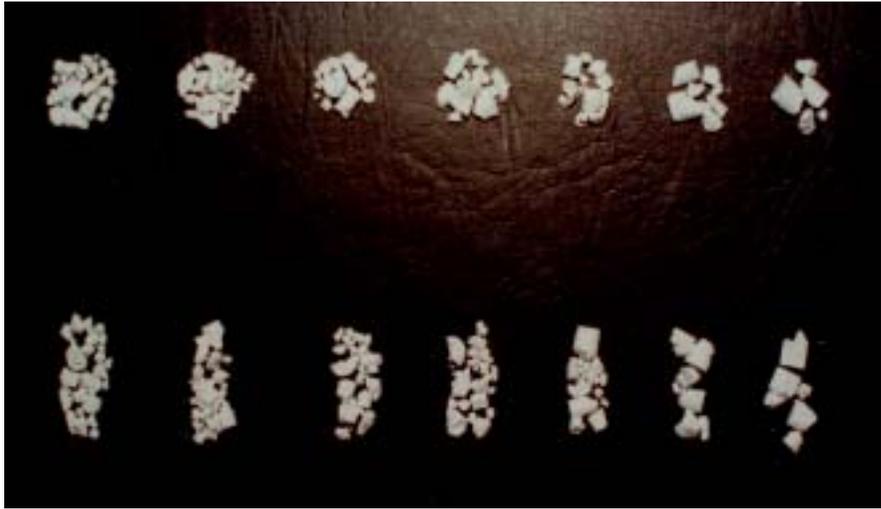
B.



3.

. B. 11mm . A. 90
500 가 가
() ()
가 .

A



B

30 50 70 90 110 130 150

4.

. A. 11mm

. B. 15mm

. A,

B

30 , 20

가

150

가

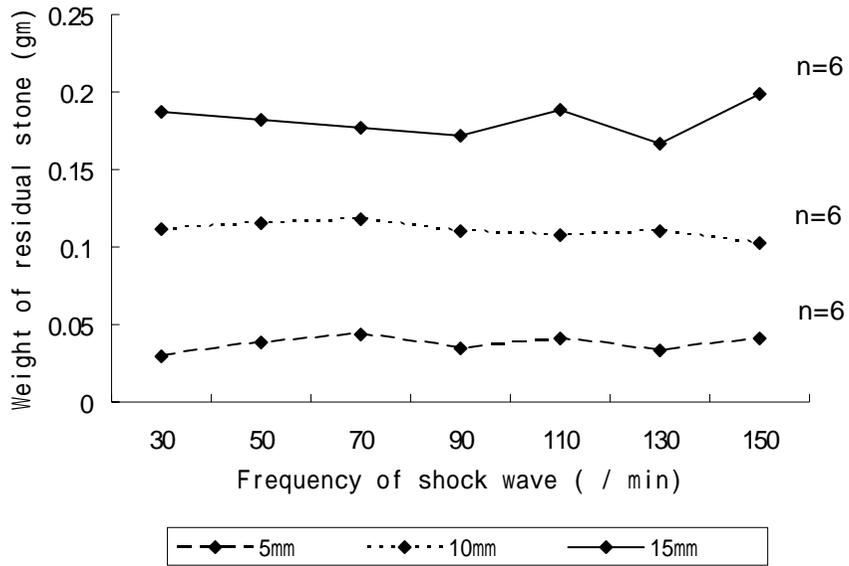
가

가

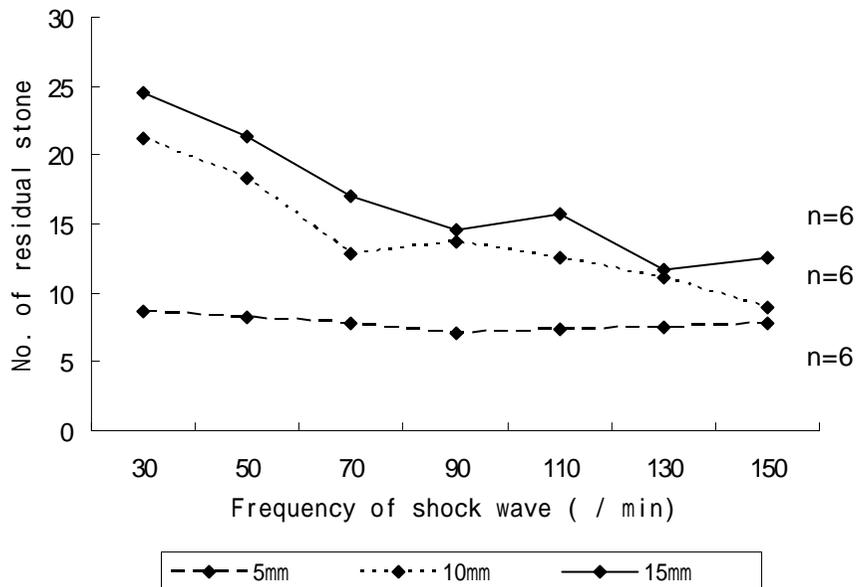
1.

()	(/min)	*	(gm)**
5mm	30	8.7 ± 1.0	0.030 ± 0.006
	50	8.2 ± 2.5	0.038 ± 0.015
	70	7.8 ± 1.5	0.043 ± 0.008
	90	7.0 ± 0.9	0.035 ± 0.005
	110	7.3 ± 1.4	0.042 ± 0.012
	130	7.5 ± 1.6	0.033 ± 0.008
	150	7.8 ± 2.2	0.042 ± 0.012
	p value	0.6917	0.2048
11mm	30	21.2 ± 3.0	0.112 ± 0.013
	50	18.3 ± 3.3	0.115 ± 0.018
	70	12.8 ± 3.5	0.118 ± 0.021
	90	13.7 ± 2.3	0.110 ± 0.020
	110	12.5 ± 2.5	0.108 ± 0.017
	130	11.2 ± 2.3	0.110 ± 0.017
	150	9.0 ± 2.7	0.102 ± 0.012
	p value	< 0.0001	0.7739
15mm	30	24.5 ± 6.3	0.187 ± 0.018
	50	21.3 ± 3.2	0.182 ± 0.021
	70	17.0 ± 2.8	0.177 ± 0.016
	90	14.5 ± 2.3	0.172 ± 0.024
	110	15.7 ± 1.9	0.188 ± 0.022
	130	11.7 ± 4.5	0.167 ± 0.025
	150	12.5 ± 3.1	0.198 ± 0.024
	p value	< 0.0001	0.2213

가 , 「one-way ANOVA test」 ,
 p value가 0.05 가 .
 *, ** : ± .



5.



6.

IV.

가

가

가

10-12

90-120

13,14

(cavitation phenomenon)

19

가

(positive pressure)

(negative pressure)

가

가

(compressive fracture)가

19

가

가

(tensile component)

가

(compressive component)

‘ spalling ’

20-22 Zhong 22

‘ spalling ’

struvite

2.7mm

(calcium oxalate monohydrate)

4.5mm

($= a_l \cdot t^*/2$; a_l :longitudinal wave speed, t^* :positive pulse duration).

가 . 2001 Eisenmenger가²³

‘ squeezing ’

30 150 20 가
 가 가 가 ()
 가 가 가 ()
 (가) () 가 가
 15mm 가 가
 가

, ‘ spalling ’

‘ squeezing ’

가

가

가

²⁴

가

^{25,26}

1 μ m

²⁷

가

(microjet)

^{28,29}

29,30

가 가 가
가 가 가
가 가 가
가 가 가

가

(2).
, ' spalling ' ' squeezing '
가

24

Huber

32,33

가

31

가 가

가

, Zeman

34

1.0 (60)

1.8 (108)

가

Lifshitz

28

Weir

17

가

가

가

가

17

가

가

가

35,36

가 가

가

,
가

가

가

V.

가 가 30 20
가 150
1. 가 ()
() 가
2. 가 가
가 가
,
3.
4. 가 가
가 가 (p<0.0001).
5. 가 50
, 50

1. Chaussy C, Schmiedt E, Jocham D, Brendel W, Forssmann B, Walther V. First clinical experience with extracorporeally induced destruction of kidney stones by shock waves. *J Urol* 1982;127:417-420.
2. Brian KA, Glenn MP. Update on shock wave lithotripsy technology. *Curr Opin Urol* 2002;12(4):287-290.
3. Clayman RVMB, Garvin TJ, Denstedt JD, Andriole GL. Lithostar: an electromagnetic acoustic shock wave unit for extracorporeal lithotripsy. *J Endourol* 1989;3:307-313.
4. Delius M, Jordan M, Eizenhoefer H, Marlinghaus E, Heine G, Liebich HG, et al. Biological effects of shock waves: kidney hemorrhage by shock waves in dogs: administration rate dependence. *Ultrasound Med Biol* 1988;14:689-694.
5. Ryan PC, Jones BJ, Kay EW, Nowlan P, Kiely EA, Gaffney EF, et al. Acute and chronic bioeffects of single and multiple doses of piezoelectric shockwaves (EDAP LT.01). *J Urol* 1991;145:399-404.
6. Zhong P, Xi X, Zhu S, Cocks FH, Preminger GM. Recent developments in SWL physics research. *J Endourol* 1999;13:611-617.
7. Delius M, Enders G, Xuan Z, Liebich HG, Brendel W. Biological effects of shock waves: kidney damage by shock waves in dogs: dose dependence. *Ultrasound Med Biol* 1988;14:117-122.
8. Willis LR, Evan AP, Lingeman JE. The impact of high-dose lithotripsy on renal function. *Contemp Urol* 1999;11:45-50.
9. Connors BA, Evan AP, Willis LR, Blomgren PM, Lingeman JE, Fineberg NS. The effect of discharge voltage on renal injury and impairment caused by lithotripsy in the pig. *J Am Soc Nephrol* 2000;11(2):310-318.
10. Winters JC, Macaluso JN Jr. Ungated Medstone outpatient lithotripsy. *J Urol* 1995;153:593-595.

11. Lingeman JE, Newman DM, Siegel YI, Eichhorn T, Parr K. Shock wave lithotripsy with the Dornier MFL 5000 lithotripter using an external fixed rate signal. *J Urol* 1995;154(3):951-954.
12. Cass AS. The use of ungating with the Medstone lithotripter. *J Urol* 1996;156:896-898.
13. Ryan FP, Ramsay LK, James EL. The effect of rate of shock wave delivery on the efficiency of lithotripsy. *Curr Opin Urol* 2002;12(4):291-295.
14. Greenstein A, Kaver I, Lechtman V, Braf Z. Cardiac arrhythmias during nonsynchronized extracorporeal shock wave lithotripsy. *J Urol* 1995;154(4):1321-1322.
15. Vallancien G, Munoz R, Borghi M, Veillon B, Brisset JM, Daudon M. Relationship between the frequency of piezoelectric shock waves and the quality of renal stone fragmentation. *Eur Urol* 1989;16(1):41-44.
16. Wiksell H, Kinn AC. Implications of cavitation phenomena for shot intervals in extracorporeal shock wave lithotripsy. *Br J Urol* 1995;75(6):720-723.
17. Weir MJ, Tariq N, Honey RJ. Shockwave frequency affects fragmentation in a kidney stone model. *J Endourol* 2000;14:547-550.
18. Robert M, Rakotomalala E, Delbos O, Navratil H. Piezoelectric lithotripsy of ureteral stones: influence of shock wave frequency on sedation and therapeutic efficiency. *J Endourol* 1999;13:157-160.
19. Lokhandwalla M, Sturtevant B. Fracture mechanics model of stone comminution in ESWL and implications for tissue damage. *Phys Med Biol* 2000;45:1923-1940.
20. Gracewski SM, Dahake G, Ding Z, Burns SJ, Everbach EC. Internal stress wave measurements in solids subjected to lithotripter pulses. *J Acoust Soc Am* 1993;94:652-661.
21. Xi XF, Zhong P. Dynamic photoelastic study of the transient stress field in solids during shock wave lithotripsy. *J Acoust Soc Am*

- 2001;109:1226-1239.
22. Zhong P, Chuong CJ, Preminger GM. Characterization of fracture toughness of renal calculi using a microindentation technique. *J Materials Sci Lett* 1993a;12:1460-1462.
 23. Eisenmenger W. The mechanisms of stone fragmentation in ESWL. *Ultrasound in Med & Biol* 2001;27(5):683-693.
 24. Zhu S, Cocks FH, Preminger GM, Zhong P. The role of stress waves and cavitation in stone comminution in shock wave lithotripsy. *Ultrasound in Med. & Biol* 2002;28(5):661-671.
 25. Sass W, Braunlich M, Dreyer H, Matura E, Folberth W, Priesmeyer H, et al. The mechanisms of stone disintegration by shock waves. *Med Biol* 1991;17:239-243.
 26. Holmer NG, Almquist LO, Hertz TG, Holm A, Lindstedt E, Persson HW, et al. On the mechanism of kidney stone disintegration by acoustic shock waves. *Ultrasound Med Biol* 1991;17:479-489.
 27. Sapozhnikov OA, Khokhlova VA, Bailey MR, Williams JC Jr, McAteer JA, Cleveland RO, et al. Effect of overpressure and pulse repetition frequency on cavitation in shock wave lithotripsy. *J Acoust Soc Am* 2002;112(3):1183-1195.
 28. Lifshitz DA, Williams JC Jr, Sturtevant B, Connors BA, Evan AP, McAteer JA. Quantitation of shock wave cavitation damage in vitro. *Ultrasound Med Biol* 1997;23(3):461-471.
 29. Howard D, Sturtevant B. In vitro study of the mechanical effects of shock-wave lithotripsy. *Ultrasound Med Biol* 1997;23:1107-1122.
 30. Field JE. The physics of liquid impact, shock wave interactions with cavities, and the implications to shock wave lithotripsy. *Phys Med Biol* 1991;36:1475-1484.
 31. Bailey MR, Blackstock DT, Cleveland RO, Crum LA. Comparison of electrohydraulic lithotripters with rigid and pressure-release ellipsoidal reflectors. II. Cavitation fields. *J Acoust Soc Am*

- 1999;106:1149-1160.
32. Huber P, Jochle K, Debus J. Influence of shock wave pressure amplitude and pulse repetition frequency on the lifespan, size and number of transient cavities in the field of an electromagnetic lithotripter. *Phys Med Biol* 1998;43:3113-3128.
 33. Huber P, Debus J, Jochle K, Simiantonakis I, Jenne J, Rastert R, et al. Control of cavitation activity by different shockwave pulsing regimens. *Phys Med Biol* 1999;44:1427-1437.
 34. Zeman RK, Davros WJ, Garra BS, Horii SC. Cavitation effects during lithotripsy. *Radiology* 1990;177:157-161.
 35. Coleman AJ, Choi MJ, Saunders JE, Leighton TG. Acoustic emission and sonoluminescence due to cavitation at the beam focus of an electrohydraulic shock wave lithotripter. *Ultrasound Med Biol* 1992;18:267-281.
 36. Jochle K, Debus J, Lorenz WJ, Huber P. A new method of quantitative cavitation assessment in the field of a lithotripter. *Ultrasound ed Biol* 1996;22:329-338.
 37. Kodama T, Takayama K. Dynamic behavior of bubbles during extracorporeal shock wave lithotripsy. *Ultrasound Med Biol* 1998;24(5):723-738.
 38. Greenstein A, Matzkin H. Does the rate of extracorporeal shock wave delivery affect stone fragmentation. *Urology* 1999;54:430-432.

Abstract

The effect of shockwave frequency on the fragmentation of stone using extracorporeal shock wave lithotripsy

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Since its introduction, extracorporeal shock wave lithotripsy(ESWL) has grown to be the most preferred choice of treatment for the stone in the upper urinary tract. In ESWL, the effectiveness of fragmentation of the stone depends on the factors such as makeup of the stone, capability of lithotripter, shockwave pressure(energy), and shockwave frequency. Among the elements that affect the fragmentation of the stone, several studies currently exist on the effect of shockwave frequency on the fragmentation of stone but to our knowledge, a little information is known on the effect of shockwave frequency for the treatment of stone. Although current studies report the effectiveness of the decreased shockwave frequency on fragmentation of the stone, there are few reports on the effectiveness of shockwave frequency for the stones of different sizes. In this study, using tube like stone receptor which is similarly shaped to the upper urinary tract, we tried to determine the most effective shockwave frequency on the fragmentation of the stone with three different sizes of stones.

In this study, three different sized stones(length: 5mm, 11mm, 15mm, diameter: 5mm) were each placed in a silicon tube(length 35mm,

diameter 6mm, thickness 1mm) and lithotripsy was performed. The total number of pulses of shockwave on 11mm and 15mm stones was 500 and on a 5mm stone, it was 400. The shockwave pressure was equally 100MPa for all. The shockwave frequency was divided 30, 50, 70, 90, 110, 130, 150 per minute and the test was repeated 6 times per different sized stones. After applying shockwave, we strained the pieces of stones in the net with 2mm holes, placed the strained stones in petri dish and dried them in 40°C oven. We measured the weight and the number of pieces of residual stones.

After ESWL, there was no statistical significance on the weight of the residual stones(5mm stone; $p=0.2048$, 11mm stone; $p=0.7739$, 15mm stone; $p=0.2213$) but there was statistical significance on the number of residual stone fragments per different sizes. For the 5mm stone, there was no statistical significance on the number of stone fragments($p=0.6917$). For the 11mm stone, as the shockwave frequency decreased, the number of stone fragments increased and it was statistically significant($p<0.0001$). It was also statistically significant for the 15mm stone($p<0.0001$). In the 11mm and 15mm stones, as the shockwave frequency decreased, the sizes of the fragmented stones were smaller and more regular. This result was shown more clearly where the shockwave frequency was 50 per minute. The sizes of residual stones were clearly larger where the shockwave frequency was 130 per minute or over.

In conclusion, the shockwave frequency does not affect the fragmentation of the stone where its size is smaller than the focus area. However, if the size of the stone is the same or larger than the focus area, the shockwave frequency of 50 per minute will fragment the stone in smaller and regular sizes and will be most effective.

Key words: shockwave lithotripsy, shockwave frequency, upper urinary

tract, fragmentation of the stone