Spontaneous healing responses of rabbit cranial defects of various sizes

Joo-Yeon Sohn

The Graduate School

Yonsei University

Department of Dental Science

Spontaneous healing responses of rabbit cranial defects of various sizes

The Master's Thesis
submitted to the Department of Dental Science
and the Graduate School of Yonsei University
in partial fulfillment of the requirements for the degree of
Master of Dental Science

Joo-Yeon Sohn

June 2010

This certifies that the dissertation thesis of Joo-Yeon Sohn is approved.

Tl	hesis Supervisor: Seong-Ho Choi
	Chang-Sung Kim
	Ui-Won Jung

The Graduate School
Yonsei University
June 2010

감사의 글

이 논문의 연구계획에서부터 완성에 이르기까지 학문적 기틀을 잡아 주시고, 논문이 완성되기까지 부족한 저를 항상 격려해 주시고 아버지와 같은 사랑과 관심으로 이끌어 주신 최성호 교수님께 깊은 감사를 드립니다. 그리고 언제나 따뜻한 관심과 조언을 아끼지 않으셨던 김종관 교수님, 채중규 교수님, 조규성 교수님, 김창성 교수님, 정의원 교수님께도 감사 드립니다.

연구와 실험 과정 내내 많은 도움을 준 엄유정, 임현창 선생님과 최은영 연구원을 비롯한 치주과 모든 의국원들에게도 감사를 드립니다.

그리고 무엇보다도 언제나 저에게 아낌없는 사랑을 주시고 힘들 때 마다 충고를 아끼지 않으신 사랑하는 부모님과 가족들에게 진정으로 사랑과 고마움의 마음을 전합니다.

.

2010년 2월

저자씀

TABLE OF CONTENTS

ABSTRACT (ENGLISH)iv
I. INTRODUCTION 1
II. MATERIALS AND METHODS4
1. The experimental design ————————————————————————————————————
2. Surgical Procedure ————————————————————————————————————
3. Evaluation 5
4. Statistics
III. RESULTS9
1. Clinical observations ————————————————————————————————————
2. Radiologic observations ······ 9
3. Histologic observations ······ 10
4. Histometric analysis · · · · 11
IV. DISCUSSION
V. CONCLUSION 19
REFERENCES 20
LEGENDS 26
TABLES 28
FIGURES 31
ABSTRACT (KOREAN) 35

LIST OF TABLES

Table 1. Defect closure (%) ······	28
Table 2. New bone area ratio (%) ······	29
Table 3. New bone ingrowth (mm) ······	30
Table 4. New bone area (mm ²) ·······	30

LIST OF FIGURES

Figure 1. Clinical Photograph of trephine burs and defect creation
Figure 2. Schematic diagram of histometric analysis and parameter
Figure 3. Radiographic view of the surgical defects at different healing period
Figure 4. Histologic views of the surgical defects at different healing period (Original magnification x10)
Figure 5. Histologic views of the newly formed bone from the defect margin in the 6mm defects (Original magnification x100)
Figure 6. Grouped-column graph showing the measurement values of the each histometric parameters

ABSTRACT

Spontaneous healing responses of rabbit cranial defects of various sizes

This study evaluated the spontaneous healing responses in surgically produced cranial defects in rabbits at different healing periods in order to determine the critical size defect (CSD) of the rabbit cranium.

Thirty-two New Zealand white rabbits were used in this study. Defects of three sizes (6, 8, and 11 mm) were created in each of 16 randomly selected rabbits, and 15-mm defects were created individually in another 16 rabbits. The defects were analyzed using radiography, histologic analysis, and histometric analysis after the animal was sacrificed at 2, 4, 8, or 12 weeks postoperatively. Four samples were analyzed for each size of defect and each healing period.

The radiographic findings indicated that defect filling gradually increased over time and that smaller defects were covered with a greater amount of radiopaque substance. Bony islands observed at 8 weeks at the center of the defect in both histologic sections and radiographs were speculated to have originated from the periosteum. In addition, the newly formed bone had matured markedly at 8 weeks. In

the 15-mm defects, which corresponds to the CSD used in many studies investigating

bone regeneration, the defect closure and new bone area ratio were 50.2±18.0%

(mean±standard deviation) and 20.1±5.9%, respectively, for the 12-week healing

period.

The new bone ingrowth and the new bone area did not differ significantly with

the defect size for the same healing period, which indicates a constant healing

capacity from the defect margin. There was a small statistically significant difference

in the defect closure and new bone area ratio between weeks 2 and 4 and between

weeks 8 and 12 in each defect group.

The results obtained for the spontaneous healing responses of rabbit cranial

defects over time and the underlying factors may provide useful guidelines for the

development of a rabbit cranial model for in vivo investigations of new bone

materials.

Keywords: Critical size defect (CSD); rabbit cranial defect; healing response; bone

regeneration

V

Spontaneous healing responses of rabbit cranial defects of various sizes

Joo-Yeon Sohn, D.D.S.

Department of Dental Science
Graduate School, Yonsei University
(Directed by Prof. Seong-Ho Choi, D.D.S., M.S.D., Ph.D.)

I. INTRODUCTION

The critical size defect (CSD) has been defined as the smallest intraosseous wound in an animal that will not heal spontaneously when left untreated for a certain time period (Bos et al., 1983) or which shows less than 10% of bone regeneration during the lifetime of the animal. (Schmitz and Hollinger, 1986) The CSD has been used as an experimental model for evaluating the effectiveness of newly developed biomaterials. (Bodde et al., 2008)

There are several bone defect models, such as those for the tibia, radius, mandible, and cranium. Among them, a cranial defect provides a model for non-load-bearing bone with relative biological inertness due to its poor blood supply and limited bone marrow, thereby resembling human mandibular bone. (Frame, 1980) Thus, cranial defects in validated small-animal models have been used in numerous studies for evaluating newly developed biomaterials for implantations prior to performing large-animal implantations. (Le Guehennec et al., 2005)

The rabbit is commonly used in animal experiments for medical research. Some of its advantages are it is easily handled, has a rapid bone turnover rate, and is fully matured within 6 months. (Gilsanz et al., 1988) Rabbit cranial defects provide a good first phase bone model for experiments related to bone graft materials and evaluations of bone regeneration due to the adequate amount of bone marrow facilitating bone formation. (Castaneda et al., 2006; Newman et al., 1995) Moreover, the rabbit has a larger cranium than the rat, which makes it possible to create multiple defects in one cranium, which reduces the operation time, cost, and observational errors between individuals.

The effects of the size and shape of rabbit cranial defects on bone and membrane materials have been reported. Some researchers have evaluated bone regeneration of rectangular (10×10 mm) cranial defects, which were used as CSDs, (Gosain et al., 2003; Pripatnanont et al., 2009) and 10-mm circular defects (Xu et al., 2008). In

addition, 8- and 6-mm circular defects have generally been used when observing the effects of barrier membranes and bone graft materials. (Hammerle et al., 1992; Kramer et al., 1968; Lundgren et al., 1992; Pallesen et al., 2002) Circular 15-mm defects also have been used as the CSD for investigating growth factors and graft materials. (Cameron, 2002; Nagata et al., 2009; Shand et al., 2002)

However, few studies have analyzed the healing capacity histometrically in defects of different sizes over time. Whilst the CSD of the rabbit cranium has been investigated previously, (Frame, 1980; Kramer et al., 1968) its size and shape have not been standardized.

Therefore, the purpose of this study was to measure the spontaneous healing responses of surgically produced cranial defects in rabbits at different healing periods in order to determine the CSD of the rabbit cranium. Information obtained from this study will be useful for making presurgical decisions related to the size and healing period of rabbit cranial defects.

II. MATERIALS AND METHODS

1. The experimental design

Thirty-two New Zealand white rabbits weighing 3.0–3.5 kg were used in this study. Defects of three sizes (6, 8, and 11 mm) were created in 16 randomly rabbits, and 15-mm defects were created individually in another 16 rabbits. The defects were analyzed after sacrificing animals at 2, 4, 8, or 12 weeks postoperatively. Four samples were analyzed for each size of defect and each healing period.

The animals were housed in separate cages under standard laboratory conditions, and fed a standard diet. Animal selection, management, surgical protocol, and preparation followed routines approved by the Institutional Animal Care and Use Committee, Yonsei Medical Center, Seoul, Korea (certification #08-267).

2. Surgical procedure

The animals were anesthetized with an intramuscular injection of a mixture of ketamine hydrochloride (Ketalar[®], Yuhan, Seoul, Korea) and xylazine (Rumpun[®], Bayer Korea, Seoul, Korea). Surgical sites were shaved and then draped with alcohol

and povidone iodine, followed by local anesthesia with 2% lidocaine (Lidocaine HCl[®], Huons, Seoul, Korea). An incision was made along the sagittal midline from the frontal bone to the occipital bone. A full-thickness flap was elevated to expose the cranial bone. Standardized circular defects with diameters of 6, 8, 11, and 15 mm were created using trephines of the corresponding sizes under cool-saline irrigation. The soft tissues were repositioned and then sutured layer by layer with a resorbable suture material (4-0 Vicryl, Ethicon, Somerville, NJ, USA) to achieve primary closure. The stitches were removed after 10 days. The animals were sacrificed at 2, 4, 8, or 12 weeks postoperatively (Figure 1).

3. Evaluation

Clinical Observation

Postoperative management included the subcutaneous administration of antibiotics (Baytril®, Bayer, Leverkusen, Germany) and the careful clinical observation of the animals throughout the healing period.

Radiologic Observation

The area of the original surgical defect and surrounding tissues were removed en bloc after sacrifice. The sections were rinsed in sterile saline and fixed in 10% buffered formalin for 10 days. After rinsing in water, all specimens were radiographed using a x-ray machine (Diox, DigiMed, Seoul, Korea) before processing for the production of histologic slides. The extent of the defects closure and newly formed radiopaque area were observed.

Histologic Observations

The sections were decalcified in 5% formic acid for 14 days and embedded in paraffin. Serial sections were cut from the center at intervals of 5 µm. The most-central sections from each block were stained with hematoxylin and eosin (H&E) and examined using light microscopy (Leica DM LB, Leica Microsystems, Wetzlar, Germany).

Histometric Analysis

Histometric measurements were made using image-analysis software (Image-Pro Plus., Media Cybernetics, Silver Spring, MA, USA). The measurement parameters are defined in the schematic diagram in Figure 2, from which the following histometric parameters were determined:

① Defect closure (%) = (total new bone ingrowth [mm])/(original defect width [mm]) \times 100 (%).

The original defect width was measured and was considered to represent 100% of the width to be analyzed.

② New bone area ratio (%) = (newly formed bone area $[mm^2]$)/(total area $[mm^2]$) × 100 (%).

The total area was determined by first identifying the external and internal surfaces of the original cranium at the right and left margins of the surgical defect, and then connecting them with lines drawn by extrapolating from their respective curvatures. This method was partly based on the work of Melo et al. (2005). The total area was taken as 100% of the area to be analyzed.

- ③ New bone ingrowth (mm) = (sum of new bone ingrowth [mm])/2.
 The average length of the new bone was measured from the right and left margins of the defect.
 - 4 New bone area (mm²).

The newly formed bone area was measured in mm²

4. Statistics

The defect closure, new bone area ratio, new bone ingrowth, and new bone area for each healing period were expressed as mean and standard-deviation values. Data were analyzed using SPSS 14.0 (SPSS Inc, Chicago, IL, USA). The significance of differences between groups with different defect sizes in relation to all of the histometric parameters were determined by the Kruskal-Wallis test followed by the Bonferroni test. The Kruskal-Wallis test was also used for comparisons between healing intervals within a single group. Statistical significance was determined at the p<0.05 level.

III. RESULTS

1. Clinical observations

All animals tolerated the surgical procedures well, and the clinical healing process was generally uneventful, with there being no dehiscence of the surgical wound, signs of inflammation, or other complications.

2. Radiographic observations

A definite defect margin was observed with a small amount of radiopacity visible along the lateral margin in all specimens at 2 weeks. At 4 weeks the defect margin was partially obscured and there were irregular and asymmetric radiopaque areas at 1.0~1.5 mm from the defect margin. The defect margins could not be distinguished and the radiopaque area extended moderately inwards for a uniform distance at 8 weeks. Some bony islets that were separated from the marginal bone were evident in the central area of the defect.

At 12 weeks the 6-mm defects were almost filled with radiopaque substance except in the central portion. In some samples a bony bridge had formed from the

marginal bone to the center, and the defect margin was no longer defined on the other diameters of the defects. The radiopaque substance extended inwards at 2.5~3.0 mm from all aspects of the margin. (Figure 3)

3. Histologic observations

A small amount of wedge-shaped bone had regenerated at 2 weeks. Most of the newly formed bone was woven bone, which showed limited bone marrow and a large number of osteoclasts. Bone regeneration was slightly greater at 4 weeks than at 2 weeks, and moderate amounts of bone regeneration and bone marrow began to appear. Active new bone formation was also present, with osteoid seams lined by plump osteoblasts.

At 8 weeks the newly formed bone had a moderate amount of bone marrow and had matured. Bone regeneration from the margin was markedly increased in both width and length. Bony islands that appeared in some specimens on the center of the defects contained moderate amounts of bone marrow. Lamellar bone was formed in the newly formed bone at 12 weeks, even in the bony islets. A bone bridge was evident in some of the specimens with 6-mm defects. (Figure 4, 5)

4. Histometric analysis

The defect closure and new bone area ratio at postoperative weeks 2, 4, 8, and 12 are listed in Table 1 and 2. The defect closure differed significantly between the 15-mm-defect group and the 6- and 8-mm-defect groups at 2 and 4 weeks after the surgery: it was 88.6±4.6% and 50.2±18.0% in the 6- and 15-mm-defect groups, respectively, at 12 weeks after the surgery. However, the defect closure did not vary significantly with the defect size at 8 weeks.

The mean new bone area ratios at 12 weeks were 53.6%, 41.8%, 35.1%, and 20.1% in the 6-, 8-, 11-, and 15-mm-defect groups, respectively. The new bone area ratio differed significantly between the 15-mm-defect group and the 6- and 8-mm-defect groups at all healing periods.

The values of the measurement parameters gradually increased over time. However, the defect closure and the new bone area ratio did not differ significantly between weeks 2 and 4 or between weeks 8 and 12 except in the 6-mm-defect group, which showed a significant difference between 8 and 12 weeks. (Figure 6)

Table 3 and 4 list the values of new bone ingrowth from the margin and new bone area, respectively. The new bone ingrowth gradually increased with the healing period, ranging from 1.30 to 1.59 mm at 2 weeks and from 2.57 to 3.00 mm at 12 weeks. However, neither the new bone ingrowth nor the new bone area differed

significantly between the groups at the same healing period.

IV. DISCUSSION

Numerous bone graft materials have been developed and evaluated using defects created in the rabbit cranium with the aim of confirming their biologic stability and osteoinductive property in clinical applications. (Cavalcanti et al., 2008; Durmus et al., 2008; Hammerle et al., 1992; Kramer et al., 1968; Lundgren et al., 1992; Torres et al., 2008; Xu et al., 2008) Investigations of the ability of bone graft materials to produce complete bone healing of a defect necessitate the use of a CSD to exclude spontaneous bony regeneration of the defect. Despite the importance of the CSD, precise analyses of spontaneous healing responses have not been discussed in the literature, and different studies have considered CSDs in the range 10–15 mm to be suitable. (Cameron, 2002; Gosain et al., 2003; Nagata et al., 2009; Pripatnanont et al., 2009; Shand et al., 2002) The present study surgically created circular defects of 6, 8, 11, and 15 mm in the craniums of New Zealand White rabbits to evaluate the spontaneous healing responses at different healing periods in order to determine the CSD.

Bone marrow began to mature and bony islets were observed after 8 weeks of healing. The defect closure and the new bone area ratio gradually increased with the healing time, but these parameters did not differ significantly between weeks 2 and 4 or between weeks 8 and 12. An observation period of at least 12 weeks was

recommended by Bodde et al. (2008) for evaluating bone formation in CSD models. Our results indicate that the healing period should be chosen according to the purpose of experiments: a healing period of 2–4 weeks could be recommended for evaluating the early phase of the healing response, such as the stability of the materials or host reactions, while 8 weeks or more may be appropriate for assessing late healing, such as bone incorporation, resorption of materials, bone remodeling, or the amount of bone regeneration.

In the 15-mm defects, which have been previously used for investigating the bone regeneration as a CSD in many studies, (Cameron, 2002; Nagata et al., 2009; Shand et al., 2002) the defect closure and new bone area ratio were 50.2±18.09% and 20.1±5.9%, respectively, at 12 weeks. To fulfill the definition of the CSD, less than 10% of bone regeneration should be observed during the lifetime of the animal, (Schmitz and Hollinger, 1986) and this period should encompass at least one complete bone-remodeling cycle. Although 15-mm defects failed to heal spontaneously at 12 weeks in the present study, they did not satisfy the definition of the CSD (Schmitz and Hollinger, 1986) since the percentage of new bone area exceeded 20%.

Many researchers have selected a defect smaller than the CSD for investigating the early events of regeneration or comparing various implant materials. (Glowacki et al., 1981; Strates and Connolly, 1989; Urist et al., 1987) It is possible to create

multiple defects in one animal when a small defect is used, which could allow the experimental testing of all materials under investigation in single animals and thereby avoid the interindividual variation. In the present study, the defect closure and new bone area did not differ significantly between the 11- and 15-mm-defect groups over the entire healing period. These findings indicate that it is possible to prepare two symmetric 11-mm defects in most rabbit craniums without involving sagittal suturing, which could be an alternative to creating one 15-mm defect especially in the midphase or late-healing period. If several materials need to be compared only for early-phase healing, four 8-mm defects could be created in a single rabbit cranium.

The new bone ingrowth ranged from 1.19 to 1.69 mm at 2 weeks and from 2.41 to 3.62 mm at 12 weeks, and did not differ significantly between the groups at the same healing period; where was also no significant intergroup difference in the new bone area. These results indicate that the healing capacity from the defect margin is constant at the same healing period regardless of the defect size. If the defect is smaller than the new bone ingrowth at a certain time of healing, the defect will be covered and filled with the new bone, and bone union will be accomplished spontaneously. Thus, the innate wound-healing potential could be one of the important factors determining the appropriate sizes of experimental defects and the healing period.

Some radiographs obtained in the present study showed bony islets in the central area of defects that were away from the defect edge. Vogeler et al. (1926) reported differences in osteogenesis between central and peripheral new bone within cranial defects, and found that regeneration in cranial defects occurred both from the cut edges of the bone and from islands of bone within the dura mater and periosteum. Periosteum provides cortical bone with a blood supply, (Bos et al., 1983; Schmitz and Hollinger, 1986) and the dura mater has been demonstrated to contribute to the reossification of cranial defects due to its osteogenic potential. (Greenwald et al., 2000) However, the dura mater can be easily damaged when creating defects, and hence the healing of cranial defects is usually accomplished from the defect edge and periosteum.

Huh et al. (2005) showed that the CSD depends on the presence of the periosteum and considered it necessary to differentiate CSDs according to whether the periosteum is present. In the present study, the dura mater of the defect was gently removed with a pincette in all of the samples so as to ensure consistent conditions, and the periosteum was repositioned and sutured with a resorbable suture material to prevent ingrowth of the soft tissue into the defects. Bony islets separate from the defect margin appeared in some samples after 8 weeks of healing, which we considered to have originated from the periosteum. It is difficult to exclude factors such as the dura mater and periosteum completely in bone regeneration, and hence

healing should be evaluated separately at the margin and central area at a certain healing period whilst considering these factors. Moreover, determining the precise CSD for the rabbit cranium requires additional experiments in which the defects are created without periosteum.

In summary, experiments designed to evaluate the effects of biomaterials in the rabbit cranium must be planned whilst carefully considering several factors that affect the healing response. The results obtained in the present study could be used to determine suitable guidelines for such experiments.

The results of the present study suggest that the CSD is larger than 15 mm, but it would be impossible to create such large defects in a single rabbit cranium. An 11-mm defect is therefore a good alternative option, since we found that none of the measurement parameters differed significantly between 11- and 15-mm defects throughout the healing period. Two 11-mm defects can be created in a single cranium without involving a sagittal suture line, thereby reducing the cost and the errors between individuals. Moreover, four 8-mm defects could be used to investigate the early-phase healing response and to simultaneously compare several materials whilst avoiding individual variation.

To evaluate the early phase of the healing response, such as the stability of the materials or the host reaction, a healing period of 2–4 weeks could be recommended. Eight weeks or more could be used to assess late healing, such as bone incorporation,

resorption of materials, bone remodeling, or the amount of bone regeneration. Moreover, since the bony islets away from the defect margin would be formed in the center of the defect after 8 weeks, bone regeneration of the central area should be evaluated separately.

The innate healing capacity that originates from the defect margin is constant regardless of the defect size. Therefore, the innate healing capacity should be considered when choosing the healing period and the defect size. In addition, when determining the appropriate experimental method, the management of dura mater and periosteum should be unified in order to obtain consistent and accurate results.

V. CONCLUSION

The present study investigated the spontaneous healing responses of rabbit cranial defects over time and the underlying factors. Within the limitations of this study, the obtained results may provide useful guidelines for the development of a rabbit cranial model for in vivo investigations of new bone materials.

REFERENCES

Bodde, E. W., Spauwen, P. H., Mikos, A. G., Jansen, J. A. 2008. "Closing capacity of segmental radius defects in rabbits". *J Biomed Mater Res A* 85(1): 206-217.

Bos, G. D., Goldberg, V. M., Powell, A. E., Heiple, K. G., Zika, J. M. 1983. "The effect of histocompatibility matching on canine frozen bone allografts". *J Bone Joint Surg Am* 65(1): 89-96.

Cameron, S. 2002. "Hand-held computers in medicine". *Can Fam Physician* 48: 111-112.

Castaneda, S., Largo, R., Calvo, E., Rodriguez-Salvanes, F., Marcos, M. E., Diaz-Curiel, M., Herrero-Beaumont, G. 2006. "Bone mineral measurements of subchondral and trabecular bone in healthy and osteoporotic rabbits". *Skeletal Radiol* 35(1): 34-41.

Cavalcanti, S. C., Pereira, C. L., Mazzonetto, R., de Moraes, M., Moreira, R. W. 2008. "Histological and histomorphometric analyses of calcium phosphate cement in rabbit calvaria". *J Craniomaxillofac Surg* 36(6): 354-359.

Durmus, E., Celik, I., Aydin, M. F., Yildirim, G., Sur, E. 2008. "Evaluation of the biocompatibility and osteoproductive activity of ostrich eggshell powder in experimentally induced calvarial defects in rabbits". *J Biomed Mater Res B Appl Biomater* 86(1): 82-89.

Frame, J. W. 1980. "A convenient animal model for testing bone substitute materials". *J Oral Surg* 38(3): 176-180.

Gilsanz, V., Roe, T. F., Gibbens, D. T., Schulz, E. E., Carlson, M. E., Gonzalez, O., Boechat, M. I. 1988. "Effect of sex steroids on peak bone density of growing rabbits". *Am J Physiol* 255(4 Pt 1): E416-421.

Glowacki, J., Altobelli, D., Mulliken, J. B. 1981. "Fate of mineralized and demineralized osseous implants in cranial defects". *Calcif Tissue Int* 33(1): 71-76.

Gosain, A. K., Santoro, T. D., Song, L. S., Capel, C. C., Sudhakar, P. V., Matloub, H. S. 2003. "Osteogenesis in calvarial defects: contribution of the dura, the pericranium, and the surrounding bone in adult versus infant animals". *Plast Reconstr Surg* 112(2): 515-527.

Greenwald, J. A., Mehrara, B. J., Spector, J. A., Chin, G. S., Steinbrech, D. S., Saadeh, P. B., Luchs, J. S., Paccione, M. F., Gittes, G. K., Longaker, M. T. 2000. "Biomolecular mechanisms of calvarial bone induction: immature versus mature dura mater". *Plast Reconstr Surg* 105(4): 1382-1392.

Hammerle, C. H., Schmid, J., Olah, A. J., Lang, N. P. 1992. "Osseous healing of experimentally created defects in the calvaria of rabbits using guided bone regeneration. A pilot study". *Clin Oral Implants Res* 3(3): 144-147.

Huh, J. Y., Choi, B. H., Kim, B. Y., Lee, S. H., Zhu, S. J., Jung, J. H. 2005. "Critical size defect in the canine mandible". *Oral Surg Oral Med Oral Pathol Oral Radiol Endod* 100(3): 296-301.

Kramer, I. R., Killey, H. C., Wright, H. C. 1968. "A histological and radiological comparison of the healing of defects in the rabbit calvarium with and without implanted heterogeneous anorganic bone". *Arch Oral Biol* 13(9): 1095-1106.

Le Guehennec, L., Goyenvalle, E., Aguado, E., Houchmand-Cuny, M., Enkel, B., Pilet, P., Daculsi, G., Layrolle, P. 2005. "Small-animal models for testing

macroporous ceramic bone substitutes". *J Biomed Mater Res B Appl Biomater* 72(1): 69-78.

Lundgren, D., Nyman, S., Mathisen, T., Isaksson, S., Klinge, B. 1992. "Guided bone regeneration of cranial defects, using biodegradable barriers: an experimental pilot study in the rabbit". *J Craniomaxillofac Surg* 20(6): 257-260.

Melo, L. G., Nagata, M. J., Bosco, A. F., Ribeiro, L. L., Leite, C. M. 2005. "Bone healing in surgically created defects treated with either bioactive glass particles, a calcium sulfate barrier, or a combination of both materials. A histological and histometric study in rat tibias". *Clin Oral Implants Res* 16(6): 683-691.

Nagata, M. J., Melo, L. G., Messora, M. R., Bomfim, S. R., Fucini, S. E., Garcia, V. G., Bosco, A. F., Okamoto, T. 2009. "Effect of platelet-rich plasma on bone healing of autogenous bone grafts in critical-size defects". *J Clin Periodontol* 36(9): 775-783.

Newman, E., Turner, A. S., Wark, J. D. 1995. "The potential of sheep for the study of osteopenia: current status and comparison with other animal models". *Bone* 16(4 Suppl): 277S-284S.

Pallesen, L., Schou, S., Aaboe, M., Hjorting-Hansen, E., Nattestad, A., Melsen, F. 2002. "Influence of particle size of autogenous bone grafts on the early stages of bone regeneration: a histologic and stereologic study in rabbit calvarium". *Int J Oral Maxillofac Implants* 17(4): 498-506.

Pripatnanont, P., Nuntanaranont, T., Vongvatcharanon, S. 2009. "Proportion of deproteinized bovine bone and autogenous bone affects bone formation in the treatment of calvarial defects in rabbits". *Int J Oral Maxillofac Surg* 38(4): 356-362.

Schmitz, J. P., Hollinger, J. O. 1986. "The critical size defect as an experimental model for craniomandibulofacial nonunions". *Clin Orthop Relat Res*(205): 299-308.

Shand, J. M., Heggie, A. A., Holmes, A. D., Holmes, W. 2002. "Allogeneic bone grafting of calvarial defects: an experimental study in the rabbit". *Int J Oral Maxillofac Surg* 31(5): 525-531.

Strates, B. S., Connolly, J. F. 1989. "Osteogenesis in cranial defects and diffusion chambers. Comparison in rabbits of bone matrix, marrow, and collagen implants". *Acta Orthop Scand* 60(2): 200-203.

Torres, J., Tamimi, F. M., Tresguerres, I. F., Alkhraisat, M. H., Khraisat, A., Lopez-Cabarcos, E., Blanco, L. 2008. "Effect of solely applied platelet-rich plasma on osseous regeneration compared to Bio-Oss: a morphometric and densitometric study on rabbit calvaria". *Clin Implant Dent Relat Res* 10(2): 106-112.

Urist, M. R., Nilsson, O., Rasmussen, J., Hirota, W., Lovell, T., Schmalzreid, T., Finerman, G. A. 1987. "Bone regeneration under the influence of a bone morphogenetic protein (BMP) beta tricalcium phosphate (TCP) composite in skull trephine defects in dogs". *Clin Orthop Relat Res*(214): 295-304.

Vogeler, K., E. Redenz, H. Walter and G. Martin: Bernard Heine's Versuche über Knochenregeneration. 1926., Springer, Berlin.

Xu, S., Lin, K., Wang, Z., Chang, J., Wang, L., Lu, J., Ning, C. 2008. "Reconstruction of calvarial defect of rabbits using porous calcium silicate bioactive ceramics". *Biomaterials* 29(17): 2588-2596.

LEGENDS

Figure 1. (a) The trephines with outer diameters of 6, 8, and 11 mm. (b) The trephine with an outer diameter of 15 mm. (c) Photograph of three created standardized circular defects with diameters of 6, 8, and 11 mm. (d) Photograph of a 15-mm defect, which included a portion of the sagittal suturing

.

- **Figure 2.** Schematic diagram of a calvarial osteotomy defect showing the measurement parameters from which the following histometric parameters were determined (with lineal and area measurements in millimeters and millimeters squared, respectively):
 - Defect closure (%): $(b1+b2)/a \times 100$
 - New bone area ratio (%): $(B1+B2)/A \times 100$
 - New bone ingrowth (mm): (b1+b2)/2
 - New bone area (mm²): B1+B2

where A represents the area within the dotted lines, corresponding to the total defect area; B1+B2 is the new bone area; and a, b1, and b2 represent the total defect width and the new bone ingrowth from the left and right margins, respectively

- Figure 3. Radiographic views of the surgical defects at different healing periods
- Figure 4. Histologic views of the surgical defects at different healing periods (H&E stain, original magnification ×10). Arrowheads point to the original defect margins, and the arrows show bony islets. Defect sizes: (a) 6 mm, (b) 8 mm, (c) 11 mm, and (d) 15 mm
- Figure 5. Histologic views of the newly formed bone from the defect margin in the 6-mm defects (H&E stain, original magnification ×100). The scale bar indicates 0.1 mm. Healing periods: (a) 2 weeks, (b) 4 weeks, (c) 8 weeks, and (d) 12 weeks
- **Figure 6.** Measured values of the histometric parameters: (a) defect closure, (b) new bone area ratio, (c) new bone ingrowth, and (d) new bone area. Data are mean and standard deviation values

TABLES

Table 1. Mean \pm SD values of the defect closure within surgically created defects (n=4)

Defect size	2 weeks	4 weeks	8 weeks	12 weeks
6 mm	43.31±9.18*aß	47.39±7.31*α	66.06±12.62°	88.57±4.52*
8 mm	40.80±9.27*°a	44.38±5.37*a	65.35±9.58	78.70±17.65
11 mm	28.67±4.51°	36.96±6.72	50.03±25.92	66.89±19.65
15 mm	$14.98\pm3.55^{\alpha\beta}$	27.67±7.24	40.83±5.85	50.15±17.99

^{*}Statistically significant difference compared to the 15-mm-defect group at the same healing period (p<0.05)

^aStatistically significant difference compared to the 12 weeks healing period at the same size defect group (p<0.05)

^BStatistically significant difference compared to the 8 weeks healing period at the same size defect group (p<0.05)

Table 2. Mean \pm SD values of the new bone area ratio (%) within surgically created defects (n=4)

Defect size	2 weeks	4 weeks	8 weeks	12 weeks
6 mm	25.59±8.18*aß	32.32±4.01*αβ	47.18±6.87*¶	53.59±6.67*¶
8 mm	22.50±5.23*aß	28.15±3.95*aß	39.21±3.11*	41.82±5.72*
11 mm	17.07±3.64°	25.63±6.13*	27.57±10.61	35.06±8.33
15 mm	5.54±2.83 ^{aB}	12.11±2.81	19.70±2.57	20.13±5.90

^{*}Statistically significant difference compared to the 15-mm-defect group at the same healing period (p<0.05)

Statistically significant difference compared to the 11-mm-defect group at the same healing period (p<0.05)

^aStatistically significant difference compared to the 12 weeks healing period at the same size defect group (p<0.05)

^{β}Statistically significant difference compared to the 8 weeks healing period at the same size defect group (p<0.05)

Table 3. Mean \pm SD values of the length of new bone ingrowth (in millimeters) within surgically created defects (n=4)

Defect size	2 weeks	4 weeks	8 weeks	12 weeks
6 mm	1.46±0.28	1.55±0.50	1.98±0.41	2.57±0.20
8 mm	1.59±0.39	1.69±0.12	2.41±0.32	2.74±0.29
11 mm	1.57±0.25	1.85±0.13	2.44±0.39	2.99±0.66
15 mm	1.30±0.26	1.77±0.26	2.30±0.34	3.00±0.58

No significant difference between groups at all healing periods (p>0.05)

Table 4. Mean \pm SD values of the new bone area (in millimeters squared) within surgically created defects (n=4)

Defect size	2 weeks	4 weeks	8 weeks	12 weeks
6 mm	1.53±0.58	1.78±0.57	2.70±0.66	3.20±0.31
8 mm	1.88±0.67	2.25±0.65	3.19±0.27	3.44±0.89
11 mm	2.27±0.67	2.75±0.93	3.88±0.96	4.03±0.69
15 mm	1.72±0.23	2.88±0.85	3.83±0.64	3.90±0.21

No significant difference between the groups at all healing periods (p>0.05)

FIGURES

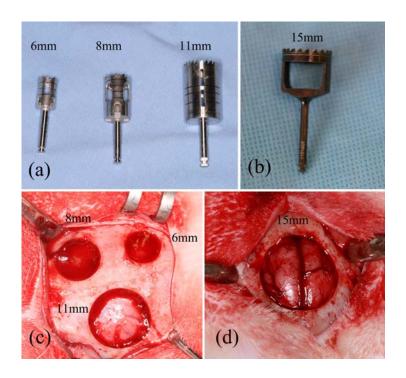


Figure 1

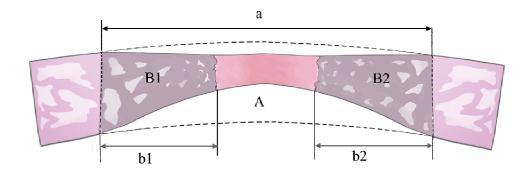


Figure 2

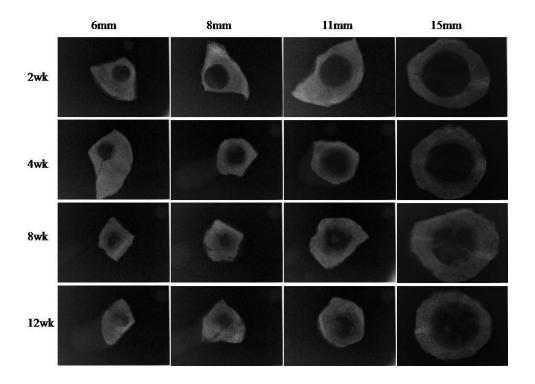


Figure 3

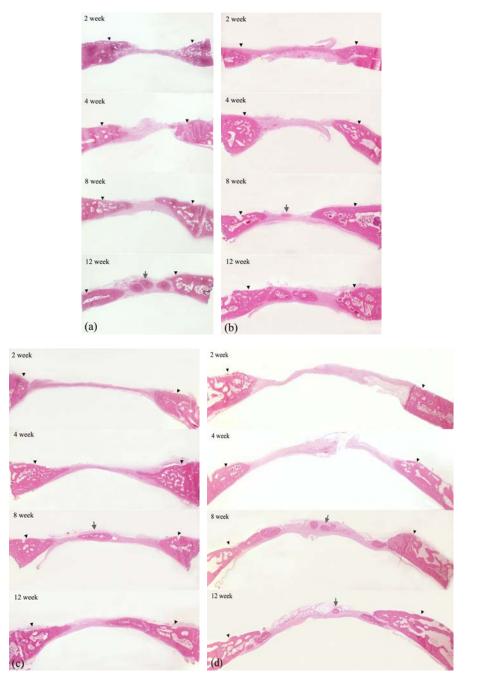


Figure 4

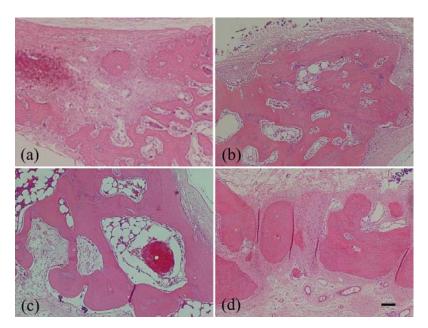


Figure 5

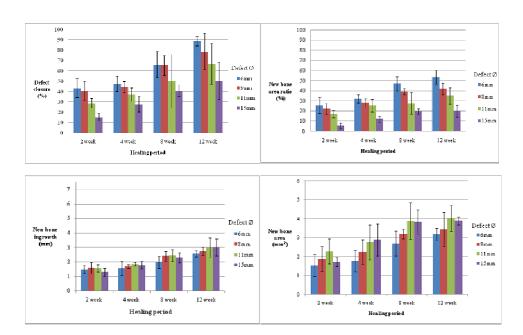


Figure 6

국문요약

토끼 두개골내 결손부의 자연치유반응

<지도교수 최 성 호>

연세대학교 대학원 치의학과

손 주 연

토끼는 의학연구를 위해 가장 많이 이용되는 실험동물 중 하나로, 토끼두개골은 골이식재의 실험에서 골재생을 평가하기 위해 적합한 모델로 골형성에 적절한 골수의 양을 가지며 쥐에 비하여 큰 두개골을 가지기때문에 한 개체 내에 여러 개의 결손부 형성이 용이하며, 이로 인해결과적으로 실험개체 수와 시간, 개체간의 오차를 줄일 수 있다는 장점이었다.

그러나 치유기간에 따른, 또한 결손부의 크기에 따른 자연적인 치유능에 대해 조직계측학적으로 분석한 연구는 아직 시행된 바 없으며, 토끼두개골에서 critical size defect에 대한 크기 및 모양에 대한 기준도 명확히 정의되지 않은 상태이다. 따라서 이번 연구의 목적은 토끼두개골에 형성된 여러 가지 크기의 결손부에서 치유기간에 따른 자연적인 치유반응에 대하여 평가 관찰하며, 토끼 두개골의 CSD에 대하여 알아보고, 이를 바탕으로 실험 설계를 위한 기준을 마련하는 데에 있다.

32마리의 New Zealand white rabbit 이 실험에 사용되었으며, 16마리의 토끼의 두개골에는 각 6, 8, 11mm 3개의 결손부를 형성하였고 나머지 16마리의 토끼 두개골에는 각 1개의 15mm 결손부를 형성하였다. 모든 크기의 defect에 대한 분석은 술 후 2, 4, 8, 12주 후로 나누어 평가하였으며, 방사선학적, 조직학적, 조직계측학적 관찰을 시행하였다.

치유 기간면에서 살펴보면, 초기치유는 2 주와 4 주 사이, 또한 8 주와 12 주 사이서 골재생량에 있어 유의할 만한 차이를 보이지 않았다. 15mm defect 는 12 주가 지나도 자연적으로 healing 되지 않는 ununion defect 이지만 약 20%의 골재생을 보여 10% 미만의 골재생이라는 CSD 의 정의에 부합되지는 않았다. 또한 시간에 따른 innate healing potential 은 defect size 에 관계없이 일정한 양을 보였으며, Dura mater 나 periosteum 의 존재에 따라 healing capacity 가 달라질 수 있음을 알 수 있었다. 그러므로 이러한 여러 가지 factor 들이 CSD 의 결정 뿐 아니라 Biomaterial 의 효과를 평가하는 데도 중요한 역할을 하기 때문에 반드시 고려해야 할 요소임을 알 수 있다.

이 연구 결과를 바탕으로 토끼 두개골에서 새로운 biomaterial 의 평가를 위한 실험을 계획하는 데 있어 Guideline 을 제시할 수 있을 것으로 사료된다.

핵심되는 말: Critical size defect(CSD); 토끼 두개골 결손부; 치유능; 골재생