

## Clinical Article

# Load Sharing Mechanism Across Graft-Bone Interface in Static Cervical Locking Plate Fixation

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**Objective :** This study is a retrospective clinical study over more than 4 years of follow up to understand the mechanism of load sharing across the graft-bone interface in the static locking plate (SLP) fixation compared with non-locking plate (NLP).

**Methods :** Orion locking plates and Top non-locking plates were used for SLP fixation in 29 patients and NLP fixation in 24 patients, respectively. Successful interbody fusion was estimated by dynamic X-ray films. The checking parameters were as follows : screw angle (SA) between upper and lower screw, anterior and posterior height of fusion segment between upper and lower endplate (AH & PH), and upper and lower distance from vertebral endplate to the end of plate (UD & LD). Each follow-up value of AH and PH were compared to initial values. Contributions of upper and lower collapse to whole segment collapse were estimated.

**Results :** Successful intervertebral bone fusion rate was 100% in the SLP group and 92% in the NLP group. The follow-up mean value of SA in SLP group was not significantly changed compared with initial value, but follow-up mean value of SA in NLP group decreased more than those in SLP group ( $p=0.0067$ ). Statistical analysis did not show a significant difference in the change in AH and PH between SLP and NLP groups ( $p>0.05$ ). Follow-up AH of NLP group showed more collapse than PH of same group ( $p=0.04$ ). The upper portion of the vertebral body collapsed more than the lower portion in the SLP fixation ( $p=0.00058$ ).

**Conclusion :** The fused segments with SLP had successful bone fusion without change in initial screw angle, which was not observed in NLP fixation. It suggests that there was enough load sharing across bone-graft interface in SLP fixation.

**KEY WORDS :** Cervical vertebrae · Spinal fusion · Surgical Fixation Devices.

## INTRODUCTION

Plate fixation combined with anterior cervical interbody fusion is a popular procedure to enhance immediate spinal stability after surgery and improve bone fusion rate. Anterior cervical plates can be classified as locking plates with static screw system (SLP) and non-locking plates (NLP) according to the presence of a lock screw system<sup>4,5,30,31</sup>. SLPs are known to have the advantages of stiff fixation, high fusion rate, and low instrument-related complication rate<sup>13,14,22,31</sup>. There is growing concern over the negative effects of the highly rigid

fixation system of SLPs, which might result in decreased load sharing across the graft-bone interface and leads to reduced fusion rates. Biomechanical results of decreased load sharing in rigid screws of SLPs have led to the introduction of various dynamic cervical plates to accommodate the axial shortening of the graft<sup>1,3,4,11,28</sup>.

In spite of the negative effects of rigid fixation of SLPs, many studies reported SLP fixation achieved high cervical interbody fusion rates without specific instrument-related complications<sup>12-14,17,18,20,22,33</sup>. Furthermore, recent clinical studies reported that the fusion rate of SLPs was similar to or even higher than dynamic plates<sup>8,29</sup>. DuBois et al.<sup>8</sup> reported that a higher rate of nonunion was actually seen in the dynamically plated patients compared to the SLPs. From these results, the authors thought that the decreased load sharing of SLPs in biomechanical tests cannot be applied to real clinical situations since the process of long-term adaptation in the human body is quite different from a biomechanical test carried out immediately after screw fixation.

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This clinical study was conducted retrospectively to identify a real mechanism of axial load sharing of SLPs by observing changes at the site of anterior interbody fusion with plate fixation over more than 4 years. To evaluate and highlight the unique mechanism of SLPs, all data were compared to those obtained from NLPs.

**MATERIALS AND METHODS**

**Patients**

This study is based on a retrospective review of patients who had undergone anterior cervical interbody fusion and plate fixation between January 1999 and December 2002. Two types of cervical plates were used : Orion plate (Medtronic Sofamor Danek, Memphis, Tennessee, USA) and Top plate (Top Surgical Products, Karlstein, Germany) for SLP and NLP fixation, respectively. Of the 53 patients who had undergone anterior cervical plate fixation, Orion plates were used in 29 and Top plates in 24. In the SLP group (male : female=17 : 12) with mean age of 44 years (20-75 years), preoperative diagnoses were 22 for degenerative diseases and 7 for traumas. In the NLP group (male : female=16 : 8) with mean age of 46 years (21-73 years), preoperative diagnoses were 16 for degenerative diseases

and 8 for traumas. We included mild subluxation trauma cases because the main objective of this study was to see the axial load transmission across the graft-bone interface. The average follow-up duration was 63 months (52-68 months) and 67 months (61-76 months) for the SLP and NLP groups, respectively (Table 1). Patients were allocated to each plate by random selection. There was no statistical difference in age and gender between the 2 groups ( $p>0.05$ ).

**Surgical procedures**

All surgical procedures were performed by the same surgeon. During surgery, patients were placed in the supine position under general anesthesia. Anterior cervical discectomy was performed using a routine Smith-Robinson technique for neural decompression. The major concern was the complete removal of the intervertebral disc and cartilaginous endplate using a high-speed drill and curettes. All patients underwent autologous tricortical iliac bone graft, which was harvested from the anterior iliac crest. Anterior cervical plates were placed after insertion of the iliac bone graft into the prepared intervertebral space and fixed by unicortical purchase using screws of 14 mm in length in both types of plates. Philadelphia neck collar was recommended to use for 1 month after surgery.

**Table 1.** Demographic and clinical characteristics of the patients

Parameters	Static locking plate (n=29)	Non-locking plate (n=24)
Gender (Male : Female)	17 : 12	16 : 8
Mean age (years)	44 (20-75)	46 (21-73)
Preoperative diagnosis		
Degenerative disease	21	16
Trauma	7	8
Level of fusion		
4/5	4	5
5/6	17	10
6/7	8	9
Mean follow-up duration (months)	63 (52-68)	67 (61-76)

**Table 2.** Description of radiological parameters

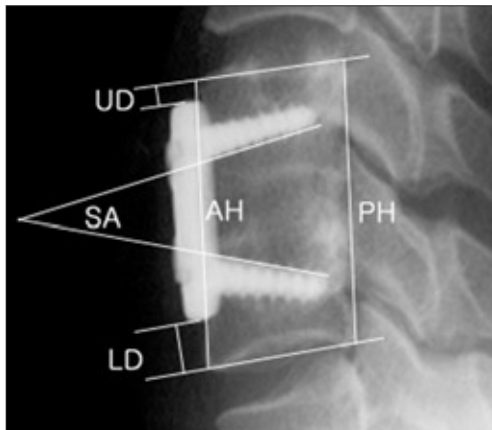
Parameter	Description
SA	Screw angle between upper and lower screws
AH	Anterior height between upper and lower endplates at anterior segment
PH	Posterior height between upper and lower endplates at posterior segment
MH	Middle height = (AH+PH)/2
UD	Upper distance between upper endplate and upper end of plate
LD	Lower distance between lower endplate and lower end of plate
dSA	Difference between initial and follow-up SA
dMH	Difference between initial and follow-up MH
dUD	Difference between initial and follow-up UD
dLD	Difference between initial and follow-up LD

**Evaluation of successful bone fusion**

An interbody bone fusion was estimated by plain cervical X-ray film with anterior-posterior and lateral flexion-extension views. The presence of mature bridging bony trabeculae between vertebrae without a lucent gap and any movement at the fused segment on flexion and extension dynamic views was accepted as a successful fusion.

**Radiological parameters**

Radiological changes in the cervical spine were estimated using plain lateral X-ray film and compared to images taken immediately after surgery. For measuring the radiological parameters, we used quantitative measurement analysis software in a picture archiving and communication system workstation (Centricity 3.0, General Electrics Medical Systems, Milwaukee, WI, USA). The checking para-



**Fig. 1.** Radiological parameters on cervical lateral X-ray film to evaluate changes at the site of interbody bone fusion with anterior cervical plate fixation. ACD & PCD : anterior and posterior cortical distance between upper and lower endplate, SA : Screw angle between upper and lower screws, UD & LD : distance from upper and lower vertebral endplate to the plate.

parameters using X-ray film were as follows : SA, AH & PH, and UD & LD (Table 2, Fig. 1).

SA was measured to see the ability to preserve initial fixation status of screws. The difference between initial and follow-up SA was defined as  $dSA$ . AH and PH were measured to detect the collapse at the anterior and posterior portions of fusion segments. Middle height (MH) of fusion segment was calculated to estimate average collapse of fusion segment :  $(AH+PH)/2$ . Each follow-up value of AH, PH, and MH was compared to initial value and described as a relative percentage (%) :  $\text{follow-up value}/\text{initial value} \times 100$ .

UD and LD were checked to detect the collapse at the upper and lower portions of fusion segment. The  $dUD$ ,  $dLD$  and  $dMH$  were defined as the difference between initial and follow-up measurements. The percentage contribution of upper and lower portions to whole fusion segment collapse was calculated by  $dUD/dMH \times 100$  and  $dLD/dMH \times 100$ , respectively.

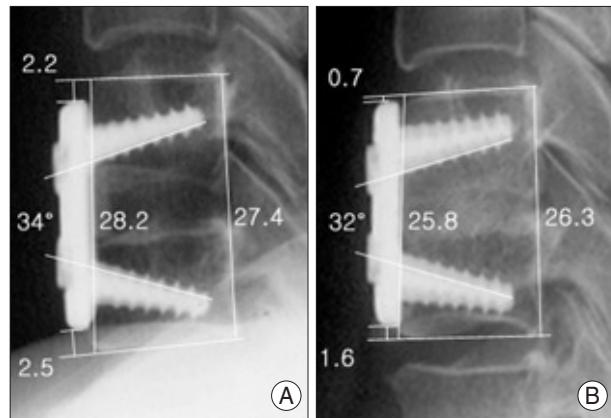
### Statistical analysis

We used SAS software for Windows (SAS version 9.1, SAS Institute Inc., Cary, NC, USA). Radiological parameters (SA, AH, MH, PH, UD, LD) were tested with Fisher's exact test. To compare fusion rates from the fused and non-fused groups, Student's 2-tailed t-test was used. Continuous variables (age and gender) of two groups were compared using Wilcoxon signed rank test. A  $p$ -value less than 0.05 was considered to be statistically significant.

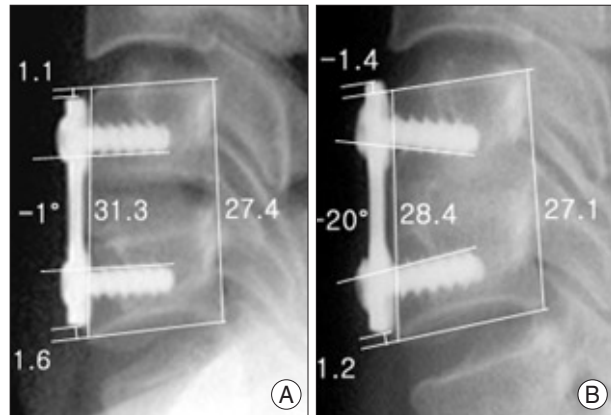
## RESULTS

### Bone fusion rate and complication

The successful intervertebral bone fusion rate was 100%



**Fig. 2.** Cervical lateral X-ray images of static locking plate (Orion plate) fixation taken immediately (A) and 61 months (B) after surgery. Migration of screws inside the vertebral body with graft collapse is noticed with a minimal change in screw angle. Upper screws migrated more than lower screws.

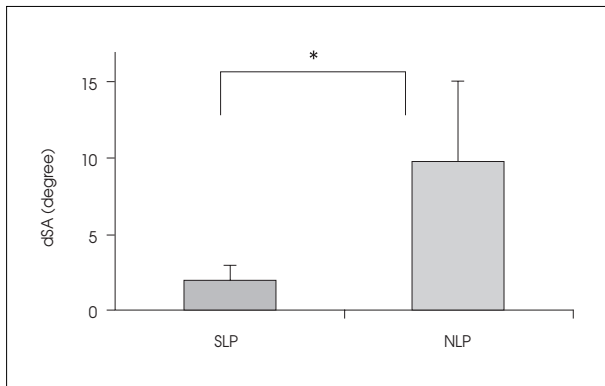


**Fig. 3.** Cervical lateral X-ray images of non-locking plate (Top plate) fixation taken immediately (A) and 65 months (B) after surgery. Breakage of screw angle at the plate-screw junction with graft collapse is noticed. Anterior part of fusion segment collapsed more than posterior part.

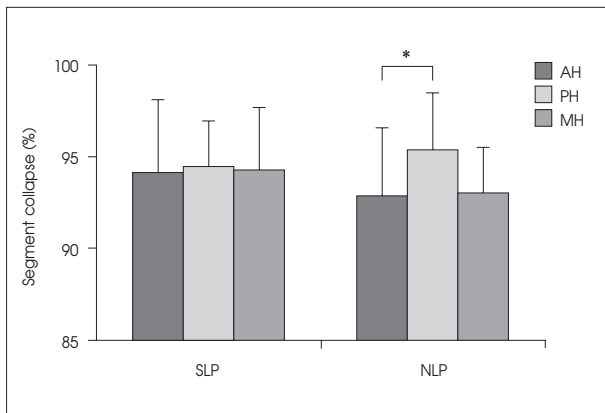
in the SLP group and 92% in the NLP group. There was no statistical difference between the fusion rates of two groups ( $p > 0.05$ ). Two patients with NLPs showed collapsed grafts with radiolucent gap in the intervertebral space. No instrument failure such as instrument breakage or screw loosening in both types of plates was found. A postoperative transient wound hematoma occurred in 1 patient after SLP fixation, which was managed by hematoma evacuation without sequelae.

### Changes in screw angle

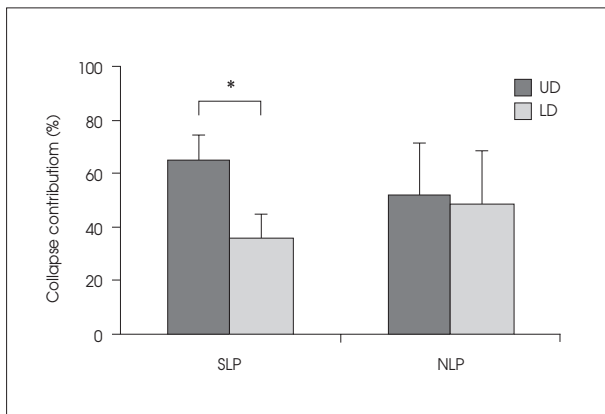
Initial SA immediately after surgery was  $32 \pm 7.6^\circ$  for SLPs and  $20 \pm 4.0^\circ$  for NLPs. At the time of follow up, SA was  $30 \pm 6.3^\circ$  for SLPs and  $11 \pm 7.9^\circ$  for NLPs. As a result,  $dSA$  was  $1.9 \pm 0.9^\circ$  in SLPs and  $9.8 \pm 5.3^\circ$  in NLPs (Figs. 2, 3, 4). The comparison of  $dSA$  between the two groups showed significant differences ( $p = 0.0067$ ).



**Fig. 4.** Difference between initial and follow-up screw angle. Screw angle of static locking plate showed little change, whereas screw angle of non-locking plate significantly changed at the follow-up ( $p=0.0067$ ). \* $p<0.05$ . NLP : non-locking plate, SA : screw angle, SLP : static locking plate.



**Fig. 5.** Collapsed anterior and posterior heights of fusion segments expressed as percentage to initial measurements. Static locking plate showed evenly decreased fusion height at the anterior and posterior parts, whereas anterior height of non-locking plate showed significantly higher collapse rate than posterior height ( $p=0.04$ ). \* $p<0.05$ .



**Fig. 6.** Percentage contribution of upper and lower portion of graft to whole fusion segment collapse. In static locking plate, contribution of the upper portion to whole graft shortening was significantly higher than in the lower portion ( $p=0.00058$ ). In non-locking plate, the collapse rate was not different between the upper and lower portion of fusion segments. \* $p<0.05$ . LD : lower distance between lower endplate and lower end of plate, UD : upper distance between upper endplate and upper end of plate.

### Changes in fused segment height

In the SLP group, follow-up AH, MH and PH were  $94.1 \pm 3.9\%$ ,  $94.2 \pm 3.4\%$  and  $94.4 \pm 2.4\%$  of initial measurements, respectively. In the NLP group, follow-up AH, MH and PH were  $92.9 \pm 3.1\%$ ,  $93.0 \pm 2.5\%$  and  $95.4 \pm 3.1\%$  of initial measurements, respectively (Figs 2, 3, 5). Statistical analysis showed that AH of NLPs showed significantly more collapse than PH of same group ( $p=0.04$ ) while SLPs showed evenly decreased fusion height at the anterior and posterior parts. In comparisons of follow-up MH between SLPs and NLPs, there was no significant difference between both groups ( $p>0.05$ ).

### Changes in upper and lower segment

The contribution of the upper and lower portion ( $dUD/dMH \times 100$  and  $dLD/dMH \times 100$ ) to whole fusion segment collapse was  $64.9 \pm 9.2\%$  and  $35.9 \pm 8.9\%$  for SLPs and  $51.6 \pm 20.1\%$  and  $48.7 \pm 19.8\%$  for NLPs, respectively (Figs. 2, 3, 6). In SLPs, the contribution of the upper portion to whole graft shortening was significantly higher than the lower portion ( $p=0.00058$ ). However, there was no significant difference between the upper and lower portions in the NLP group.

## DISCUSSION

Anterior plate fixation after cervical discectomy and fusion has gained broad support because of excellent initial stability, increased fusion rates, decreased requirements for external immobilization, and an early return to work<sup>1,5,14,21,24</sup>. In biomechanical test of cervical plates, SLPs significantly increased the rigidity of the tested screw-plate systems initially and after cyclic loading compared to NLPs<sup>31</sup>. In clinical areas, SLPs have been used more frequently than NLPs in recent years and they are known to be safe and simple instrumentation with unicortical purchase of screws with high fusion rate, strong stability, and low instrument-related failure rate<sup>2,14,20,23,24</sup>.

Despite well-known clinical data on SLPs, the concept of decreased load sharing of rigid locking screw system was suggested in biomechanical test, and dynamic plates with semi-rigid variable angle screws or controlled settling system along the graft axis have been introduced to accommodate the shortening of the graft<sup>1,3,4,7,11,28</sup>. As far as the authors are concerned, there has been no clinical study about decreased load sharing of SLPs, except the biomechanical test. In this study, compared to the NLPs with toggling screws, SLPs allowed sufficient load sharing across the graft-bone interface without any change in initial screw fixation status.

In the biomechanical test by Brodke et al.<sup>3)</sup>, load sharing

of Orion locking plates was much lower than dynamic cervical plates. We thought that decreased load sharing in their biomechanical test was correct because load sharing was measured immediately after screw insertion into an artificial plastic vertebral body. However, in real clinical situations, screws are inserted into the vertebral body, which is mainly composed of cancellous bone, and an intravertebral adaptation occurs between the screw and vertebral body accompanied by continuous load sharing across the graft-bone interface in the fusion segment. During adaptation time, screws migrate along the vertical axis inside the vertebral body without breakage of initial screw angle. We call this “intravertebral screw migration”. As far as we are aware, there has not been any reports about this concept of load sharing mechanism in SLPs. The authors think that continuous load sharing with progressive vertical migration of screws explains the high fusion rate without instrumental failure in SLPs.

Our study showed that, with regard to graft collapse in middle height, there was no significant difference between SLPs and NLPs. This means that the shortness of a graft occurs in both plate systems at similar collapse rates. However, the mechanism of graft collapse was quite different. In NLPs with toggling screws, the axial load was transmitted through a breakage of initial screw angle at the screw-plate junction. On the contrary, SLPs screws kept their initial status while the intervertebral graft collapsed evenly at the anterior and posterior portions. We think that early breakage of the screw angle in NLPs is a possible cause of more anterior graft collapse than posterior portion, which will result in postoperative segmental kyphosis. In the aspect of the sagittal balance of the vertebral column, the collapse rate at the anterior or posterior fusion segments is important because postoperative kyphotic angulation has adverse effects on clinical outcome<sup>5,18,30</sup>. This study reveals the possible mechanism of high postoperative segmental kyphosis in NLP fixation compared to SLP as indicated in previous reports<sup>19,24,32</sup>.

Successful intervertebral bone fusion is closely related to clinical results. The reported fusion rates differ by various methods : 88-92% for interbody fusion without instrumentation, 87-99% for interbody fusion with NLP fixation, and 95-100% for interbody fusion with SLP fixation<sup>5,6,10,17,18,25,27,33</sup>. In the present study, SLPs showed 100% of interbody fusion rate. We believe that excellent fusion rates of SLPs can also be explained by firmly fixed fusion segments and continuous load sharing.

This study showed 5-6% in graft collapse rate via “intravertebral migration of screws” in SLPs. If fusion levels were more than one, the collapsed portion would be longer with

resultant increase in intravertebral screw migration. In such cases, screws may even migrate into the disc space if they are inserted near the adjacent disc space. An inappropriate long plate can result in contact of the plate tip with the disc space, which consequently affects disc degeneration and anterior bony spur formation on the adjacent segment<sup>16,26</sup>. We suggest that SLP screws with the shortest plate length should be inserted as near to the fusion site as possible.

A contribution of upper or lower fusion segments to the whole collapse is another considerable factor in anterior cervical instrumentation. Studies on adjacent segments after cervical fusion have reported that significant increases in intradiscal pressure and segmental motion occur at levels adjacent to fusion during normal range of motion<sup>9,26</sup>. Intradiscal pressure and segmental motion were increased more at the upper than lower segment, especially during neck flexion<sup>9,26</sup>. In our study, the upper fusion segment collapsed more than the lower segment, which may be affected by the greater load on the upper segment with resultant increase in intravertebral screw migration. It suggests that more attention should be paid to upper screw insertion when using SLP in multilevel fusion.

This study has a limitation in the use of plain X-ray films to estimate the morphological changes at fusion segment after plate fixation. For observation of the changes inside the vertebral body during intravertebral screw migration, additional CT scanning would be better. However, this study shows the mechanism how axial load transmits to the interbody graft in anterior cervical fixation using SLP. Concurrent mechanisms of rigid screw fixation and axial load transmission to the graft explain the excellent fusion and low instrumentation failure rates. SLP is still considered a good choice for anterior cervical fixation after interbody fusion according to our results.

## CONCLUSION

This study has significance by showing the possible mechanism of load sharing in SLP fixation. SLPs transmitted axial load by the mechanism of intravertebral screw migration without change in initial status of screw fixation, which resulted in successful intervertebral bone fusion. In NLPs, load sharing was achieved through early breakage of screw angle at the screw-plate junction, and anterior part of the graft collapsed more than posterior part. The collapse rate of the fusion segment was not significantly different between SLPs and NLPs.

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